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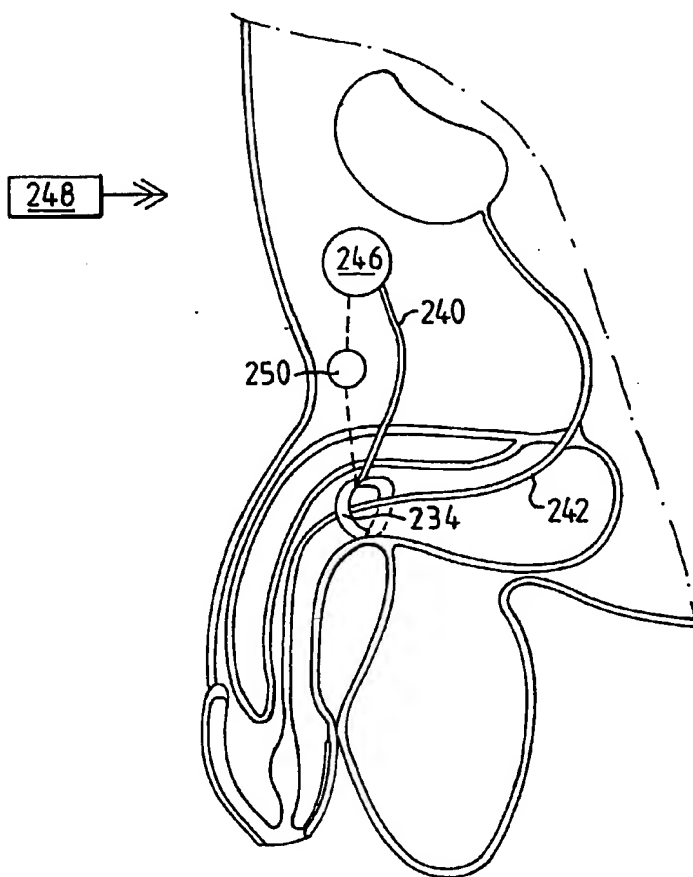
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[Continued on next page]

(54) Title: HYDRAULIC URINARY INCONTINENCE TREATMENT APPARATUS



(57) Abstract: A urinary incontinence treatment apparatus comprises an adjustable restriction device (234) implanted in a patient, who suffers from urinary incontinence. The restriction device engages the urethra (244) of the patient to restrict, i.e. to close the urine passageway. An implanted adjustment device is adapted to adjust the restriction device such that the urethra is temporarily released, in order to open the urine passageway when the patient wants to urinate. An implanted powered hydraulic operation device (246) operates the adjustment device.

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HYDRAULIC URINARY INCONTINENCE TREATMENT APPARATUS

The present invention relates to a urinary incontinence
5 treatment apparatus, comprising an adjustable restriction
device adapted to engage the urethra or urine bladder of a
patient, who suffers from urinary incontinence, to form a
restricted urine passageway in the urethra or urine bladder.
An implantable adjustment device is provided for adjusting the
10 restriction device to restrict the urethra or urine bladder to
close the urine passageway, or release the urethra or urine
bladder to open the urine passageway, when the restriction
device is implanted in the patient. An implantable operation
device is provided for operating the adjustment device.

15 Urine incontinence is a widespread problem. Many people
are helped through training of the muscles in the pelvic floor
but too many have severe problems with urine leakage. Many
different solutions to this problem have been tried. There is
a prior manually operated sphincter system connected to an
20 elastic reservoir/pump placed in the scrotum or in the region
of the labia majora. A disadvantage of this system is that
over time hard fibrosis is developed around the reservoir
which may cause malfunction of pumping components and it is
rather complicated to manually squeeze the elastic reservoir
25 when urinating, especially woman can get their fingers wet.
Thus, the created fibrosis will sooner or later become a hard
fibrotic layer which may make it difficult to pump the
reservoir. Yet a further disadvantage is that the use of
hydraulic fluid always entails a risk of fluid leaking from
30 the prosthesis. Furthermore, it is a rather complicated task
to manually pump the reservoir when needing to urinate.

A prior hydraulic device which is made for compressing

the urethra is disclosed in U.S. Pat. No. 5520606. Prosthetic sphincters with an inflatable cuff which surrounds the urethra or encloses it on two sides are disclosed in for example U.S. Pat. Nos. 4571749 and 4222377. U.S. Pat. No. 5 4969474 discloses a hydraulic method for treating both men and women with urinary incontinence problem in the same way. The apparatus of the U.S. Pat. No. 4969474 includes a reservoir containing fluid and an inflatable compression device that will compress urethra without risking tissue loss or necrosis 10 to occur. An artificial hydraulically operated urethral sphincter employing an external magnet to achieve closure of the urethral cuff is disclosed in U.S. Pat. Nos. 5562598. A prior mechanical prosthetic sphincter, disclosed in U.S. Pat. No. 4619245 comprises a manually controllable actuating 15 component for implanting at a convenient location in the patients body.

A prime object of the present invention is to provide a urinary incontinence treatment apparatus, which does not 20 require manual manipulation of a combined reservoir and pump mechanism placed in the scrotum or in the region of the labia majora of the patient.

Another object of the invention is to provide an urinary incontinence treatment apparatus, which does not require 25 complicated surgery.

Yet another object of the invention is to provide an urinary incontinence treatment apparatus, which may be conveniently controlled by the patient with a remote control.

These objects are obtained by an apparatus of the kind 30 described initially characterised in that the operation device comprises a powered operation device and/or a servo means.

The expression "powered" should be understood as

energised with everything without manual force, preferably electric energy. In other words, the adjustment device is operated in a non-manual manner. The expression "non-manual manner" should be understood to mean that the adjustment
5 device is not operated by manually touching subcutaneously implanted components of the apparatus or not manipulated by touching the skin of the patient. Thus, as opposed to prior practice when treating urine incontinence, the adjustment device of the invention is not operated by manual forces, such
10 as by manually compressing a fluid containing balloon implanted in the scrotum or in the region of labia majora. Of course, manual manipulation of a subcutaneous start button or the like for activating the powered operation device is permitted within the scope of the present invention.

15 Alternatively, or in combination with a powered operation device, the servo means may be used, which enables manual manipulation without need for strong manipulation forces. The servo means may comprise hydraulic means, electric control means, magnetic means, or mechanical means, which may be
20 activated by manual manipulating means. Using a servo system will save the use of force when adjusting the adjustment device, which may be of importance in many applications.

The term "servo means" encompasses the normal definition of a servo mechanism, i.e. an automatic device that controls
25 large amounts of power by means of very small amounts of power, but may alternatively or additionally encompass the definition of a mechanism that transfers a weak force acting on a moving element having a long stroke into a strong force acting on another moving element having a short stroke. The
30 servo means may comprise a motor, preferably an electric motor, which may be reversible.

In accordance with a main embodiment of the invention,

the apparatus comprises a reservoir, preferably containing a predetermined amount of hydraulic fluid, also implantable in the patient, wherein the operation device, suitably electrically powered, operates the adjustment device by using
5 the hydraulic fluid of the reservoir.

The adjustment device may comprise an expandable cavity in the restriction device, wherein the urethra or urine bladder is squeezed upon expansion of the cavity and released upon contraction of the cavity. In this embodiment the
10 operation device is adapted to distribute hydraulic fluid from the reservoir to expand the cavity, and from the cavity to the reservoir to contract the cavity.

A fluid distribution tube may readily be connected between the reservoir and the cavity in a manner so that the
15 tube does not interfere with other implanted components of the apparatus.

Preferably, the reservoir defines a chamber for the predetermined amount of fluid and the operation device changes the volume of the chamber. The operation device suitably
20 comprises first and second wall portions of the reservoir and is adapted to provide relative displacement between the first and second wall portions of the reservoir, in order to change the volume of the chamber.

The operation device may be adapted to provide said
25 relative displacement in response to the pressure in the reservoir. Suitably, the operation device comprises a pressure controlled hydraulic operation device. For safety, an alarm may be provided for generating an alarm signal in response to the lapse of a predetermined time period during which the
30 pressure controlling the hydraulic operation device exceeds a predetermined high value.

Suitably, the operation device is adapted to distribute

fluid from the reservoir to the cavity of the restriction member in response to a predetermined first displacement of the first wall portion of the reservoir relative to the second wall portion of the reservoir and may distribute fluid from
5 the cavity to the reservoir in response to a predetermined second displacement of the first wall portion relative to the second wall portion.

The first and second wall portions of the reservoir may be displaceable relative to each other by a magnetic,
10 hydraulic, or electric power means, such as an electric motor. In this embodiment no pump is used, only the volume of the reservoir is varied. This is of great advantage compared to the solution described below when the operation device comprises a pump used to pump fluid between the reservoir and
15 the adjustment device because there is no need for a non-return valve and it is still possible to have fluid going both to and from the reservoir. Thus, the significant risk of malfunction when using such a non-return valve implanted in the patient is eliminated.

20 The operation device may comprise hydraulic means and a fluid conduit extending between the hydraulic means and the adjustment device. The hydraulic means and conduit are devoid of any non-return valve. The reservoir may form part of the conduit and a fluid chamber with a variable volume. The
25 operation device may distribute fluid from the fluid chamber to the adjustment device by reduction of the volume of the chamber and withdraw fluid from the adjustment device by expansion of the volume of the chamber. The operation device preferably comprises a motor for moving a movable wall of the
30 reservoir for changing the volume of the chamber. Any kind of motor could be used for the different operations as well as wireless remote solutions for controlling the operations.

The restriction device preferably is operable to perform a reversible function and accordingly there is a reversing device implantable in the patient for reversing the function performed by the restriction device. Such a reversing function preferably involves enlarging and restricting the urine passageway by the restriction device, suitably in a stepless manner. In this connection, the control device suitably controls the reversing device, which may include a switch, to reverse the function performed by the restriction device. The reversing device may comprise hydraulic means including a valve for shifting the flow direction of a fluid in the hydraulic means. Alternatively, the reversing device may comprise a mechanical reversing device, such as a switch or a gearbox.

Where the reversing device comprises a switch the control device suitably controls the operation of the switch by shifting polarity of released energy supplied to the switch. The switch may comprise an electric switch and the source of energy may supply electric energy for the operation of the switch. The switch mentioned above may comprise an electronic switch or, where applicable, a mechanical switch.

Where the operation device comprises a motor, the reversing device is adapted to reverse the motor.

In accordance with another particular embodiment of the invention, the operation device comprises a pump for pumping fluid between the reservoir and the adjustment device. A mechanical solution is proposed in which it is possible to pump fluid from the reservoir to the adjustment device and vice versa just by pushing an activation member in one direction. The pump preferably comprises a first activation member for activating the pump to pump fluid from the reservoir to the adjustment device, and a second activation

member for activating the pump to pump fluid from the adjustment device to the reservoir. At least one of the first and second activation members may be operable by manual manipulation, preferably to permit manual pushing, pulling or rotation thereof in one direction, or by a device powered magnetically, hydraulically, or electrically (e.g. by an electric motor), or be operable by a combination of these methods. Suitably, at least one of the activation members may be adapted to operate when subjected to an external pressure exceeding a predetermined magnitude.

Another alternative is a pump pumping in only one direction and an adjustable valve to change the direction of fluid to either increase or decrease the amount of fluid in the reservoir. This valve may be manipulated either manually, mechanically, magnetically, or hydraulically.

The main embodiment of the invention described above including the reservoir may alternatively be equipped with a servo means comprising a reverse servo. The term "reverse servo" is to be understood as a mechanism that transfers a strong force acting on a moving element having a short stroke into a weak force acting on another moving element having a long stroke; i.e. the reverse function of the above-defined alternative mechanism of a normal servo mechanism. A first closed hydraulic system that controls another closed hydraulic system in which hydraulic means of the adjustment device is incorporated may be used. Minor changes in the amount of fluid in a smaller reservoir of the first system could then be transferred by the reverse servo into major changes in the amount of fluid in a larger reservoir in the second system. In consequence, the change of volume in the larger reservoir of the second system affects the hydraulic means of the adjustment device. For example, a short stroke that decreases

the volume of the smaller reservoir will cause the larger reservoir to supply the adjustment device with a large amount of hydraulic fluid, which in turn results in a long mechanical adjustment stroke on the restriction device.

5 The great advantage of using such a reverse servo is that the larger volume system could be placed inside the abdomen or retroperitoneum where there is more space and still it would be possible to use manual manipulation means of the smaller system subcutaneously. The smaller reservoir could be
10 controlled directly or indirectly by a fluid supply means. The fluid supply means may include another small reservoir, which may be placed subcutaneously and may be activated by manual manipulation means. Both the normal servo means and the specific reverse servo may be used in connection with all of
15 the various components and solutions described in the present specification.

 Thus, the reverse servo may be adapted to provide relative displacement between the first and second wall portions of the reservoir, suitably in response to the
20 pressure in the reservoir, in order to change the volume of the chamber of the reservoir.

 Generally, the servo means, including the reverse servo, comprises a pressure controlled servo means. The alarm mentioned above may alternatively be adapted to generate an
25 alarm signal in response to the lapse of a predetermined time period during which the pressure controlling the servo means exceeds a predetermined high value.

 The reverse servo may comprise magnetic means, electric means or manual manipulation means or a combination thereof.
30 Preferably, however, the reverse servo comprises hydraulic means.

 In accordance with a particular embodiment of the

invention, the reverse servo further comprises a servo reservoir defining a chamber containing servo fluid, and the operation device comprise first and second wall portions of the servo reservoir, which are displaceable relative to each other to change the volume of the chamber of the servo reservoir. The first and second wall portions of the servo reservoir may be displaceable relative to each other by magnetic means, hydraulic means, or electric control means.

Where the reverse servo comprises hydraulic means it may further comprise a fluid supply reservoir connected to the servo reservoir in a closed system and containing a further predetermined amount of fluid. The fluid supply reservoir defines a chamber for the further predetermined amount of fluid and the operation device is adapted to change the volume of the chamber and thereby control the amount of fluid in the servo reservoir. The fluid supply reservoir comprises first and second wall portions, which are displaceable relative to each other to change the volume of the chamber of the fluid supply reservoir. Suitably, the fluid supply reservoir increases the amount of fluid in the servo reservoir in response to a predetermined first displacement of the first wall portion of the fluid supply reservoir relative to the second wall portion of the fluid supply reservoir and decreases the amount of fluid in the servo reservoir in response to a predetermined second displacement of the first wall portion of the fluid supply reservoir relative to the second wall portion of the fluid supply reservoir.

In accordance with an embodiment of the invention, the adjustment device comprises a hydraulic adjustment device, and an implantable reservoir containing a predetermined amount of hydraulic fluid and a conduit providing fluid connection between the reservoir and the hydraulic adjustment device are

provided. The operation device is adapted to operate the hydraulic adjustment device by distributing hydraulic fluid through the conduit between the reservoir and the hydraulic adjustment device, wherein the conduit and hydraulic adjustment device are devoid of any non-return valve to permit free flow of hydraulic fluid in both directions in the conduit. Preferably, the reservoir forms a fluid chamber with a variable volume, and the operation device is adapted to distribute fluid from the chamber to the adjustment device by reduction of the volume of the chamber and to withdraw fluid from the adjustment device by expansion of the volume of the chamber. The operation device may comprise a motor or a pump. Alternatively, the operation device may comprise a movable wall of the reservoir for changing the volume of the chamber. For example, the operation device may be adapted to change the volume of the chamber by moving the movable wall in response to the pressure in the chamber.

In the above embodiments including a reservoir for hydraulic fluid an injection port may be provided for subcutaneous implantation in the patient to be in fluid communication with the chamber of the reservoir. The injection port may be integrated in the reservoir. Such an injection port may be provided for enabling, normally single, once-and-for-all, calibration of the amount of fluid in the hydraulic system used.

In the various embodiments hereinafter described the restriction device generally forms an at least substantially closed loop. However, the restriction device may take a variety of different shapes, such as the shape of a square, rectangle or ellipse. The substantially closed loop could for example be totally flat, i.e. thin as seen in the radial direction. The shape of restriction device may also be changed

during use, by rotation or movements of the restriction device in any direction. A physical lumen, like the urethra or urine bladder, often is easier to restrict by contracting two opposite sidewalls of the lumen against each other. Thus, the
5 restriction device may be designed to perform such a contracting effect of the opposite walls of the urethra or urine bladder. Either mechanical or hydraulic solutions may be employed to operate the restriction device. Alternatively, the restriction device may comprise an adjustable cuff, a clamp or
10 a roller for bending or rotating the urethra or urine bladder to close its passageway. Such a cuff, clamp or roller may also be utilized for squeezing the urethra or urine bladder against human material inside the body of the patient, for example the sacral bone of the patient, or against implanted structures of
15 the apparatus. The bending or rotating members may take any shape and be either hydraulic or non-inflatable.

Preferably the restriction device comprises an elongated restriction member and forming means for forming the restriction member into at least a substantially closed loop
20 around the urethra or urine bladder, wherein the loop defines a restriction opening, whereby the adjustment device adjusts the restriction member in the loop to change the size of the restriction opening.

Advantageously, the forming means may form the
25 restriction member into a loop having a predetermined size. Alternatively, the forming means may form the restriction member into a loop having a size selected from several predetermined sizes.

The adjustment device may change the size of the
30 restriction opening such that the outer circumferential confinement surface of the restriction member either is changed or is unchanged.

The elongated restriction member may be flexible, for example take the shape of a belt or cord, and the adjustment device may pull a first portion of the flexible restriction member from a second portion of the flexible restriction member opposite the first portion in the loop to squeeze the urethra or urine bladder between the opposite lengths of the elongated flexible restriction member to restrict the urine passageway. The restriction member may be non-inflatable, and the adjustment device may mechanically adjust the restriction member in the loop.

The adjustment device may mechanically or hydraulically adjust the restriction device. In the embodiments described the adjustment device may either mechanically or hydraulically adjust the restriction device, where applicable. It should be noted that the operation device might mechanically or hydraulically operate the adjustment device irrespectively of whether the adjustment device is adapted to adjust the restriction device mechanically or hydraulically.

In accordance with an embodiment of the invention, the restriction device comprises at least two elements on opposite or different sides of the urethra or urine bladder, and the adjustment device decreases the distance between the elements to squeeze the urethra or urine bladder between the elements, thereby restricting the urine passageway. It is also possible to use only one element and squeeze the urethra or urine bladder against human bone or tissue. The elements above may as well as all the restriction members mentioned in this application be everything from rigid to soft.

In accordance with an alternative, the restriction device bends or rotates a portion of the urethra or urine bladder to restrict the urine passageway in the same. For example, the restriction device may comprise at least two bending members,

such as cylindrical or hour-glass shaped rollers, positioned on opposite or different sides of the urethra or urine bladder and displaced relative to each other along the urethra or urine bladder, and the adjustment device may move the bending
5 members against the urethra or urine bladder to bend the latter to restrict the urine passageway. The restriction device may also rotate a portion of the urethra or urine bladder. The bending or rotating members may take any shape and be either hydraulic or non-inflatable.

10 Alternatively, the two bending members one placed more distal than the other may be rotated in opposite directions relative to each other. With interconnecting means for example flexible bands between the bending members a restriction will occur between the bending members when they are rotated.

15 Preferably the adjustment device is operable to adjust the restriction device to steplessly change the restriction of the urine passageway in the urethra or urine bladder.

All embodiments according to the invention may be controlled by a wireless remote control.

20 In accordance with an advantageous embodiment of the invention, there is provided a wireless remote control for non-invasively controlling the operation device. The remote control may conveniently comprise an external hand-held remote control unit, which is manually operable by the patient to
25 control the restriction device to squeeze and release the urethra or urine bladder. With the wireless remote control the apparatus of the invention is conveniently controlled by the patient when he so desires, which is of great advantage compared to the prior art procedures. With the remote control
30 the apparatus of the invention is conveniently controlled to adjust the implanted restriction device to release the urine passageway when the patient wants to relieve himself or

herself.

The remote control may advantageously be capable of obtaining information related to important parameters, such as the condition of the urine passageway or the pressure against the restriction device, and of commanding the operation device to operate the adjustment device to adjust the restriction device in response to obtained information. With the remote control the apparatus of the invention is conveniently controlled to adjust the implanted restriction device to open and close the urine passageway. The adjustment device may control the restriction device to steplessly change the restriction of the passageway.

Preferably, the wireless remote control comprises a separate signal transmitter or receiver and a signal receiver or transmitter implanted in the patient. For example, the signal transmitter and signal receiver may transmit and receive a signal in the form of digital pulses, which may comprise a magnetic or electric field. Alternatively, which is preferred, the signal transmitter and signal receiver may transmit and receive an electromagnetic wave signal, a sound wave signal or a carrier wave signal for a remote control signal. The receiver may comprise an implanted control unit for controlling the adjustment device in response to a control signal from the signal transmitter. Any known or conventional signal transmitting or signal receiving means that is suitable for use with a human or mammal patient may be provided as the signal transmitter or signal receiver.

The apparatus of the invention may further comprise an implanted energiser unit for providing energy to energy consuming implanted components of the apparatus, such as electronic circuits and/or a motor for operating the adjustment device. Where a motor is provided the control unit

is adapted to power the motor with energy provided by the energiser unit in response to a control signal received from the signal transmitter. The motor may be any type of motor, such as a pneumatic, hydraulic or electric motor and the energiser unit may power the motor with pressurized gas or liquid, or electric energy, depending on the type of motor. Where the motor is an electric motor, it may power pneumatic or hydraulic equipment.

The remote control advantageously comprises wireless energy transfer device for transferring energy from outside the patient's body to energy consuming implantable components of the apparatus. The energy transfer device may comprise said energiser unit is adapted to transform energy from the control signal, as it is transmitted to the signal receiver, into electric energy. Where the operation device comprises a motor the wireless energy transfer device is adapted to directly power the motor with transferred energy.

The energy transferred by the wireless energy transfer device preferably comprises a signal, suitably a wave signal. The energy transferred by the wireless energy transfer device may comprise an electric field or a magnetic field or a combination thereof. The signal may be analog or digital or a combination thereof. The energy transfer device may transfer the energy from the signal into a direct, pulsating direct or alternating current or a combination thereof.

Any of the above mentioned signals may comprise analog or digital pulses. The analog or digital signal may comprise a magnetic field or an electric field or a combination thereof. Where the signal is a wave signal it may comprise an electromagnetic wave signal, a sound wave signal or a carrier wave signal for a remote control signal or a combination thereof. Where a carrier signal is used it may be frequency,

amplitude or frequency and amplitude modulated.

The apparatus of the invention may comprise an implantable source of energy for powering the operation device and/or for energizing other energy consuming components of the apparatus, wherein the energy from the source of energy is releasable from outside the patient's body. Furthermore, the apparatus may comprise an energy transmission device for wireless transmission of energy of a first form and an energy transforming device implantable in the patient for transforming the energy of the first form into energy of a second form, to be supplied to the source of energy and/or other implantable energy consuming parts of the apparatus. The energy transforming device may transform the wireless energy directly or indirectly into energy different than the wireless energy for operation of the restriction device. Typically, the energy of the second form is different than the energy of the first form. The function of the energy transmission device may be different from that of the energy transforming device.

An implantable motor or pump for operating the adjustment device may be provided, wherein the energy transmission device may be adapted to transmit wireless energy in the form of a magnetic field or electromagnetic waves or field for direct power of the motor or pump, as the wireless energy is being transmitted. Suitably, the energy transmission device transmits energy by at least one signal separate from the above mentioned control signal.

An implantable stabiliser for stabilising the energy of the first or second form may be provided. Where the energy of the second form comprises electric current, the stabiliser suitably comprises at least one capacitor.

Generally, the source of energy comprises a battery, accumulator, capacitor or a combination thereof.

In accordance with an embodiment of the invention, the apparatus comprises a control device adapted to produce wireless energy for directly powering the operation device and/or for energizing other energy consuming components of the
5 apparatus.

It should be understood that the energy consuming parts of the apparatus for example a motor or pump may be or may not be energised with the unchanged wirelessly transmitted energy as this being transmitted as well as being or not being
10 energised with energy different than the transmitted energy for example transformed into electrical energy but still directly used for energising the energy consuming parts of the apparatus as the transmitted energy is transmitted. Alternatively the energy consuming parts of the apparatus may
15 be energised from a implanted source of energy or storage device, which still may be loaded with wireless energy. In all these aspects it is preferable to be able to wirelessly control the release of energy and get an feedback of the result of the performed function of the device. Direct use of
20 transmitted energy may be unreliable without a feedback what has happened, has the energy reached it's goal?

Generally, the wireless energy may comprise a wave signal including a sound wave signal, an ultrasound wave signal, an electromagnetic wave signal, an infrared light signal, a
25 visible light signal, an ultra violet light signal, a laser light signal, a micro wave signal, a radio wave signal, an x-ray radiation signal or a gamma radiation signal.

Any of the above mentioned signals may comprise a wave signal including a sound wave signal, an ultrasound wave
30 signal, an electromagnetic wave signal, an infrared light signal, a visible light signal, an ultra violet light signal, a laser light signal, a micro wave signal, a radio wave

signal, an x-ray radiation signal or a gamma radiation signal.

The control device may be adapted to produce wireless energy in the form of a train of energy pulses and the energy transfer device may be adapted to intermittently transfer the
5 train of energy pulses for direct use in connection with the energising of the energy consuming components of the apparatus. Alternatively, the control device may be adapted to control the energy transforming device to produce the energy of the second form in said train of energy pulses for direct
10 use in connection with the operation of the adjustment device. The transferred energy preferably comprises electric energy. An implantable capacitor may be provided for producing the train of energy pulses.

Where a capacitor is used in any of the above described
15 embodiments it may have a relatively low capacity, i.e. less than 0,1 μF , in order to be small and suited for implantation.

Where the operation device comprises an implantable motor or pump for operating the adjustment device, the energy transfer device may be adapted to directly power the motor or
20 pump with transferred energy, at the same time as the energy is transferred. Where a pump is used it should not be a plunger type of pump, because a plunger pump is noisy, but may comprise a peristaltic or membrane pump.

As mentioned above the apparatus comprises a wireless
25 remote control for non-invasively controlling the operation device, which preferably is electrically powered. Alternatively, the operation device is powered by magnetic energy, non-magnetic energy, electromagnetic energy, non-electromagnetic energy, kinetic energy, non-kinetic energy,
30 sonic energy, non-sonic energy, thermal energy or non-thermal energy. However, the operation device may be unpowerable by permanent static magnetic energy. Any other kind of energy,

such as electric, electromagnetic energy or a moving permanent magnetic energy, may be conceivable for operating the adjustment device. As a result, the implanted restriction device would not be accidentally adjusted if the patient comes
5 close to any permanent magnet. Suitably, the operation device is adapted to non-invasively operate the adjustment device.

Where the operation device comprises a hydraulic operation device it may use hydraulic fluid, the viscosity of which changes when the hydraulic fluid is exposed to energy,
10 preferably electric energy, different than thermal energy. However, use of hydraulic fluid of the kind having a viscosity that increases when exposed to heat or a magnetic field, i.e. the hydraulic fluid would not become substantially more viscous when exposed to heat or influenced by magnetic forces,
15 should be avoided, because external heat sources or heat from the body when the patient has fever and external magnetic sources might affect the implanted components of the apparatus.

The adjustment device is may be operable to adjust the
20 restriction device to steplessly change the restriction of the urine passageway. Furthermore, the adjustment device may be adapted to mechanically adjust the restriction device. Alternatively, it may be adapted to hydraulically adjust the restriction device by using hydraulic means, which is devoid
25 of hydraulic fluid of the kind having a viscosity that substantially increases when exposed to heat or a magnetic field.

In accordance with an embodiment of the invention, the apparatus comprises a control device for controlling the
30 restriction device. The control device may comprise an internal programmable control unit implantable in the patient and, possibly an external control unit outside the patient's

body for programming the programmable internal control unit. Alternatively, the external control unit may be programmable and wirelessly control the restriction device. The control device may be adapted to produce wireless energy for directly
5 powering the operation device and/or for energizing other energy consuming components of the apparatus.

At least one sensor for sensing at least one physical parameter of the patient may conveniently be implanted in the patient. The sensor may preferably sense as the physical
10 parameter the horizontal position of the patient or may comprise a pressure sensor for sensing the pressure against the restriction device or the urethra or urine bladder or other important parameters. The pressure sensor may be any suitable known or conventional pressure sensor such as shown
15 in U.S. patents 5540731, 4846181, 4738267, 4571749, 4407296 or 3939823; or an NPC-102 Medical Angioplasty Sensor.

Either the internal control unit or the external control unit of the control device may suitably control the restriction device to enlarge or close the urine passageway.
20 For safety the restriction device may enlarge or open the urine passageway in response to the sensor sensing for example an abnormally high pressure value. The internal control unit may directly control the restriction device in response to signals from the sensor.

25 Wherever magnetic means is utilized according to the invention it may comprise a permanent magnet and a magnetic material reed switch, or other suitable known or conventional magnetic means.

Where a source of energy is used the control device
30 suitably is operable from outside the patient's body for controlling the source of energy to release energy for use in connection with the operation of the adjustment device, when

the adjustment device is implanted. The source of energy may be provided external to the patient's body, and the control device may be adapted to control the external source of energy to release wireless energy for use in connection with the
5 operation of the adjustment device.

The control device may control the source of energy to release magnetic energy, non-magnetic energy, electromagnetic energy, non-electromagnetic energy, kinetic energy, non-kinetic energy, sonic energy, non-sonic energy, thermal energy
10 or non-thermal energy, preferably in a non-invasive manner and for a determined time period and/or in a determined number of energy pulses.

Where the implantable components of the apparatus comprise electrical electrical components they may include at
15 least one or a single voltage level guard. In this case, the electrical components suitably are devoid of any current detector and/or charge level detector. Furthermore, the electrical components may comprise a capacitor or accumulator, wherein the charge and discharge of the capacitor or
20 accumulator is controlled by use of the voltage level guard. As a result, there is no need for any implanted current detector and/or charge level detector for the control of the capacitor, which makes the apparatus simple and reliable.

In accordance with an advantageous embodiment of the
25 invention, the apparatus comprises an implantable switch for directly or indirectly switching the operation of the restriction device. The switch may be operated by the energy supplied by the energy transmission device mentioned above to switch from an off mode, in which the implantable source of
30 energy mentioned above is not in use, to an on mode, in which the source of energy supplies energy for the operation of the restriction device.

In accordance with an alternative embodiment, the above mentioned a remote control may be employed for controlling the implantable source of energy, wherein the switch is operated by the energy supplied by the energy transmission device to switch from an off mode, in which the remote control is prevented from controlling the source of energy and the source of energy is not in use, to a standby mode, in which the remote control is permitted to control the source of energy to supply energy for the operation of the restriction device.

10 In accordance with another alternative embodiment, the switch is operated by the energy supplied by the implantable energy transforming device mentioned above to switch from an off mode, in which the source of energy is not in use, to an on mode, in which the source of energy supplies energy for the operation of the restriction device.

In accordance with yet another alternative embodiment, the switch is operated by the energy supplied by the energy transforming device to switch from an off mode, in which the remote control is prevented from controlling the source of energy and the source of energy is not in use, to a standby mode, in which the remote control is permitted to control the source of energy to supply energy for the operation of the restriction device.

Suitably, the restriction device is embedded in a soft or gel-like material, such as a silicone material having hardness less than 20 Shore.

The energy transforming device may be designed to be implanted subcutaneously or in the abdomen, thorax or cephalic region of the patient.

30 The adjustment device may be adapted to adjust the restriction device such that the restriction device provides a predetermined contraction of the urine passageway that is

satisfactory for the patient.

The adjustment device is preferably adapted to adjust the prosthesis device in a non-flux magnetic or non-thermal manner or non-viscosity changing manner, because these would give
5 rise to unreliable function of the device. The expression "non-viscosity changing manner" should be understood to mean that the adjustment device is not adjusted by changing the viscosity of the hydraulic fluid used.

All the above described various components, such as the
10 motor, pump and capacitor, may be combined in the different embodiments where applicable. Also the various functions described in connection with the above embodiments of the invention may be used in different applications, where applicable. Specifically, the various remote control functions
15 described and all the various methods for supplying energy may be used in any conceivable combination that is apparent to those skilled in the art.

The invention also provides a method for treating a patient suffering from urinary incontinence, comprising the
20 steps of placing at least two laparascopical trocars in the body of a patient suffering from urinary incontinence, inserting a dissecting tool through the trocars and dissecting an area of the urethra or urine bladder in the abdominal or pelvic or retroperitoneal surroundings, placing at least one
25 adjustable restriction device in the dissected area engaging the urethra or urine bladder adjusting the restriction device to normally restrict the urine passageway in the urethra or urine bladder, and adjusting the restriction device to open the urine passageway when the patient wants to relieve himself
30 or herself. A hydraulic adjustable restriction device may be used when practicing this method, preferably in a non-manual manner, i.e. without touching subcutaneously implanted

components of the apparatus.

The method may further comprise implanting a source of energy in the patient and providing a control device for controlling the source of energy from outside the patient's body to supply energy for the adjustment of the restriction device.

The present invention also provides a method for treating urinary incontinence, comprising surgically implanting in the body of a patient suffering from urinary incontinence an adjustable restriction device engaging the urethra or urine bladder to restrict the urine passageway, and when desired to allow the patient to urinate, adjusting the restriction device to temporarily release the urethra or urine bladder to open the urine passageway. The method may further comprise implanting an elongated restriction member of the restriction device around the urethra or urine bladder.

The urinary incontinence treatment apparatus of the invention may also be laparoscopically implanted. Thus, there is provided a method comprising the steps of placing at least two laparoscopical trocars in the patient's body, inserting a dissecting tool through the trocars and dissecting an area of the pelvic or abdominal or retroperitoneal surroundings and placing an operable restriction device in the dissected area, so that the restriction device engages the urethra or urine bladder to restrict the urine passageway.

The invention is described in more detail in the following with reference to the accompanying drawings, in which

FIGURES 1A-D are block diagrams of four different principal embodiments of the urinary incontinence treatment apparatus according to the invention.

FIGURE. 2A-D are cross-sectional views of a pump mechanism according to Fig. 1C, which is designed to pump fluid in opposite directions by mechanically pushing a wall portion in only one direction.

5 FIGURE 3 is a cross-sectional view of a reservoir having a variable volume controlled by a remote control motor, in accordance with a particular embodiment of the principal embodiment shown in Fig. 1B or 2B.

10 FIGURE 4 is a cross-sectional view of a reservoir having a variable volume adjustable by manual manipulation, in accordance with a particular embodiment of the principal embodiment shown in Fig. 1B or 1D.

15 FIGURE 5A is a perspective view of a hydraulic, pneumatic or mechanical servo system in accordance with a particular embodiment of the principal embodiment shown in Fig. 1D.

FIGURE 5B is a cross-sectional view taken along line VB-VB of Fig 5A.

FIGURE 6 is a block diagram illustrating remote control components of the device of the invention;

20 FIGURE 7 is a schematic view of exemplary circuitry used for the block diagram in Fig. 4;

FIGURE 8 is a schematic view of a band with a cavity defining a restriction opening for use in accordance with the invention.

25 FIGURES 9A and 9B are schematic views of a first mechanical restriction device for use in accordance with the invention;

30 FIGURES 10A and 10B are schematic views of a second mechanical restriction device for use in accordance with the invention;

FIGURE 11 is a schematic view of a third mechanical restriction device for use in accordance with the invention;

FIGURE 12A is a schematic front view of a fourth mechanical restriction device for use in accordance with the invention;

FIGURES 12B and 12C are sectional views along the line A-A of FIGURE 12A;

FIGURES 13A through 17B are five modifications of the embodiment of FIGURES 12A-12C;

FIGURE 18 is a view of an inflatable restriction device of the apparatus of the invention: and

FIGURE 19 illustrates the apparatus of the invention implanted in a patient.

Referring to the drawing figures, like reference numerals designate identical or corresponding elements throughout the several figures.

Figs. 1A-D is a block diagram of four different embodiments of the urinary incontinence treatment apparatus according to the invention. Fig. 1A shows an elongated restriction member in the form of a band 2 forming a loop which defines a restriction opening. The band 2 provides a restricted urine passageway in the urethra when applied around the latter. Fig. 1A further shows a separate reservoir 4, a one way pump 6 and an alternate valve 8. Fig. 1B shows the band 2 and a fluid supply reservoir 10. Fig. 1C shows the band 2, a two way pump 12 and the reservoir 4. Fig. 1D shows a servo system with a first closed system controlling a second system. The servo system comprises the fluid supply reservoir 10 and a servo reservoir 14. The servo reservoir 14 controls a larger adjustable reservoir 16 which in connection with the band 2 applied around the urethra varies the volume of a cavity in the band, which in turn varies the restricted urine passageway in the urethra. Such a band 2 forming the

restriction opening 3 is illustrated schematically in Fig. 8. The band 2 comprises an adjustment device having an expandable/contractable cavity 5 which is expanded or contracted by supplying hydraulic fluid (e.g. from reservoir 4, 6, 10, or 16), and the band 2 may be sutured in place, illustrated schematically at 7 in Fig.8.

Figs. 2A-D are cross-sectional views of a pump mechanism adapted to pump fluid in both directions only by mechanically pushing a separate sealing wall portion 18 in one direction. Fig. 2A shows a piston 20 pushed forwards against a spring 22 towards the wall portion 18 and located in a pump housing 24 conducting fluid from a right upper fluid passage 26 of the housing 24 to a left fluid passage 28 of the housing 24. A main valve 30 is open and a nonreturn valve 32 is closed. Fig. 2B illustrates the first pump movement in which the piston 20 has moved forwards and reaches the wall portion 18. Fig. 2C illustrates how the piston 20 moves backwards by the action of the spring 22. The main valve 30 is now closed and the nonreturn valve 32 is open for fluid from the right upper passage 26. Fig. 2D illustrates how the piston 20 is moved further downwards from its position according to Fig. 2B while pushing the wall portion 18 downwardly against a second spring 34 that is stronger than spring 22, whereby fluid escapes from a right lower fluid passage 36. When moving the piston 20 backwardly from the position according to Fig. 2D, fluid enters the left fluid passage 28 and a valve 38 in the lower right fluid passage 36 closes.

Fig. 3 is a cross-sectional view of a reservoir 40 defining a chamber 42, the volume of which is variable by an operation device in the form of a remote controlled electric motor 44, in accordance with Fig. 1B or 1D. The reservoir 40 and the motor 44 are placed in a housing 46. The chamber 42 is

varied by moving a large wall 48. The wall 48 is secured to a nut 50, which is threaded on a rotatable spindle 52. The spindle 52 is rotated by the motor 44 via an angular gearing, which comprises two conical gear wheels 54 and 56 in mesh with each other. The motor 44 is powered by a battery 58 placed in the housing 46. An signal receiver 60 for controlling the motor 44 is also placed in the housing 46. Alternatively, the battery 58 and the signal receiver 60 may be mounted in a separate place. The motor 44 may also be powered by energy transferred from transmitted signals.

Fig. 4 is a cross-sectional view of a reservoir 62 defining a chamber 64, the volume of which is variable and is controlled by manual manipulation. A gable wall portion 66 of an open ended inner cylindrical housing 68 is adapted to be pushed downwards to fit in a desired locking groove 70 of a plurality of locking grooves 70 on the mantle wall of the cylindrical housing 68, to reduce the volume of the chamber 64. The inner cylindrical housing 68 is suspended by springs 72 and is telescopically applied on an outer cylindrical housing 74. When pushing the inner cylindrical housing 68 it moves downwards relative to the outer cylindrical housing 74 causing the gable wall portion 66 to release from the locking groove 70 and move upwards relative to the inner cylindrical housing 68. When the inner housing 68 is moved upwardly by the action of the springs 72 the volume of the chamber 64 is increased.

Figs. 5A and 5B show a servo means comprising a main ring-shaped fluid reservoir 76 defining a chamber 78, the volume of which is variable. Centrally positioned in the main ring-shaped reservoir 76 there is a servo fluid reservoir 80 defining a chamber 82, the volume of which is variable. The chamber 82 of the servo reservoir 80 is substantially smaller

than the chamber 78 of the main reservoir 76. The two reservoirs 76 and 80 are situated between two opposite separate walls 84 and 86, and are secured thereto. When changing the amount of fluid in the servo reservoir 80, the
5 two opposite walls 84,86 are moved towards or away from each other, whereby the volume of the chamber 78 of the main reservoir 76 is changed.

Fig. 6 shows the basic parts of a remote control system of the apparatus of the invention including the electric motor
10 44 of the embodiment shown in Fig. 3. In this case, the remote control system is based on the transmission of electromagnetic wave signals, often of high frequencies in the order of 100 kHz - 1 GHz, through the skin 130 of the patient. In Fig.6, all parts placed to the left of the skin 130 are located
15 outside the patient's body and all parts placed to the right of the skin 130 are implanted. Any suitable remote control system may be used.

An external signal transmitting antenna 132 is to be positioned close to a signal receiving antenna 134 implanted
20 close to the skin 130. As an alternative, the receiving antenna 134 may be placed for example inside the abdomen of the patient. The receiving antenna 134 comprises a coil, approximately 1-100 mm, preferably 25 mm in diameter, wound with a very thin wire and tuned with a capacitor to a specific
25 high frequency. A small coil is chosen if it is to be implanted under the skin of the patient and a large coil is chosen if it is to be implanted in the abdomen of the patient. The transmitting antenna 132 comprises a coil having about the same size as the coil of the receiving antenna 134 but wound
30 with a thick wire that can handle the larger currents that is necessary. The coil of the transmitting antenna 132 is tuned to the same specific high frequency as the coil of the

receiving antenna 134.

An external control unit 136 comprises a microprocessor, a high frequency electromagnetic wave signal generator and a power amplifier. The microprocessor of the control unit 136 is adapted to switch the generator on/off and to modulate signals generated by the generator to send digital information via the power amplifier and the antennas 132,134 to an implanted control unit 138. To avoid that accidental random high frequency fields trigger control commands, digital signal codes are used. A conventional keypad placed on the external control unit 136 is connected to the microprocessor thereof. The keypad is used to order the microprocessor to send digital signals to either increase or decrease the size of the restriction opening defined by the loop of the restriction member 2. The microprocessor starts a command by applying a high frequency signal on the antenna 132. After a short time, when the signal has energized the implanted parts of the control system, commands are sent to increase or decrease the size of the restriction opening of the restriction member 2 in predefined steps. The commands are sent as digital packets in the form illustrated below.

Start pattern, 8 bits	Command, 8 bits	Count, 8 bits	Checksum, 8 bits
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The commands are sent continuously during a rather long time period (e.g. about 30 seconds or more). When a new increase or decrease step is desired the Count byte is increased by one to allow the implanted control unit 138 to decode and understand that another step is demanded by the external control unit 136. If any part of the digital packet

is erroneous, its content is simply ignored.

Through a line 140, an implanted energizer unit 126 draws energy from the high frequency electromagnetic wave signal received by the receiving antenna 134. The energizer unit 126
5 stores the energy in a power supply, such as a large capacitor, powers the control unit 138 and powers the electric motor 44 via a line 142.

The control unit 138 comprises a demodulator and a microprocessor. The demodulator demodulates digital signals
10 sent from the external control unit 136. The microprocessor of the control unit 138 receives the digital packet, decodes it and, provided that the power supply of the energizer unit 126 has sufficient energy stored, sends a signal via a signal line 144 to the motor 44 to either increase or decrease the size of
15 the restriction opening of the restriction member 2 depending on the received command code.

Alternatively, the energy stored in the power supply of the energizer unit may only be used for powering a switch, and the energy for powering the motor 44 may be obtained from
20 another implanted power source of relatively high capacity, for example a battery. In this case the switch is adapted to connect the battery to the control unit 138 in an "on" mode when the switch is powered by the power supply and to keep the battery disconnected from the control unit in a "standby"
25 mode when said switch is unpowered.

With reference to Fig. 7, the remote control system schematically described above will now be described in accordance with a more detailed embodiment. The external control unit 136 comprises a microprocessor 146, a signal
30 generator 148 and a power amplifier 150 connected thereto. The microprocessor 146 is adapted to switch the signal generator 148 on/off and to modulate signals generated by the signal

generator 148 with digital commands that are sent to implanted components of the urinary incontinence apparatus. The power amplifier 150 amplifies the signals and sends them to the external signal transmitting antenna 132. The antenna 132 is
5 connected in parallel with a capacitor 152 to form a resonant circuit tuned to the frequency generated by the signal generator 148.

The implanted signal receiving antenna coil 134 forms together with a capacitor 154 a resonant circuit that is tuned
10 to the same frequency as the transmitting antenna 132. The signal receiving antenna coil 134 induces a current from the received high frequency electromagnetic waves and a rectifying diode 160 rectifies the induced current, which charges a storage capacitor 158. A coil 156 connected between the
15 antenna coil 134 and the diode 160 prevents the capacitor 158 and the diode 160 from loading the circuit of the signal receiving antenna 134 at higher frequencies. Thus, the coil 156 makes it possible to charge the capacitor 158 and to transmit digital information using amplitude modulation.

20 A capacitor 162 and a resistor 164 connected in parallel and a diode 166 forms a detector used to detect amplitude modulated digital information. A filter circuit is formed by a resistor 168 connected in series with a resistor 170 connected in series with a capacitor 172 connected in series with the
25 resistor 168 via ground, and a capacitor 174, one terminal of which is connected between the resistors 168, 170 and the other terminal of which is connected between the diode 166 and the circuit formed by the capacitor 162 and resistor 164. The filter circuit is used to filter out undesired low and high
30 frequencies. The detected and filtered signals are fed to an implanted microprocessor 176 that decodes the digital information and controls the motor 44 via an H-bridge 178

comprising transistors 180,182,184 and 186. The motor 44 can be driven in two opposite directions by the H-bridge 178.

The microprocessor 176 also monitors the amount of stored energy in the storage capacitor 158. Before sending signals to
5 activate the motor 44, the microprocessor 176 checks whether the energy stored in the storage capacitor 158 is enough. If the stored energy is not enough to perform the requested operation, the microprocessor 176 waits for the received signals to charge the storage capacitor 158 before activating
10 the motor 44.

Figs. 9A and 9B show an embodiment of the apparatus of the invention comprising a restriction device 202 having an elongated flexible restriction member 204, such as a belt, a cord or the like. The flexible member 204 extends in a loop
15 around the urethra. (Alternatively, the flexible member 204 may comprise two separate parts on opposite sides of the urethra.) One portion 204A of member 204 is attached to a frame 208 and another portion 204B of member 204 opposite portion 204A in the loop of the flexible member 204 is
20 connected to an adjustment device 210, which is fixed to the frame 208. The adjustment device 210 pulls the flexible member 204 away from portion 204A to squeeze the urethra between two opposite lengths of the flexible member 204 to thereby restrict the urine passageway, see Fig. 96A, and
25 releases the urethra from the flexible member 204 to thereby increase the urine passageway, see Fig. 9B.

Figs. 10A and 10B show an embodiment of the apparatus of the invention comprising a restriction device 212 having two plate or bar elements 214 on opposite sides of the urethra
30 206. An adjustment device 216 moves the elements 212 in parallel towards each other to squeeze the urethra 206 between the elements 212 to thereby restrict the urine passageway, see

Fig. 10A, and moves the elements 212 away from each other to enlarge the urine passageway, see Fig. 10B.

Fig. 11 shows an embodiment of the apparatus of the invention comprising a restriction device 218 having two articulated clamping elements 220 positioned on opposite sides of the urethra 206. An adjustment device 222 moves the clamping elements 220 toward each other to clamp the urethra 206 between the clamping elements 220 to thereby restrict the urine passageway, and moves the clamping elements 220 away from each other to release the urethra 206 from the clamping elements 220 to thereby enlarge the urine passageway.

Figs. 12A, 12B and 12C show an embodiment of the apparatus of the invention comprising a restriction device 224 having three bending members in the form of cylindrical rollers 226, 228 and 230 displaced relative one another in a row along the urethra 206 and positioned alternately on opposite sides of the urethra 206. (Alternatively, each roller 226, 228 and 230 may take the shape of an hour-glass.) An adjustment device 232 moves the two outer rollers 226, 230 laterally against the urethra 206 in one direction and the intermediate roller 228 against the urethra 206 in the opposite direction to bend the urethra to thereby restrict the urine passageway, see Fig. 12B. To release the urethra from the rollers 226-230, the adjustment device 232 moves the rollers 226-230 away from the urethra 206, see Fig. 12C.

Figs. 13A through 17B schematically illustrates modifications of the above embodiment according to Figs. 12A-12C. Thus, Figs. 13A and 13B show an embodiment similar to that of Figs. 12A-12C except that the bending members are oval and not rotatable. Figs. 14A and 14B show an embodiment similar to that of Figs. 13A and 13B except that the oval bending members are rotatable to squeeze the urethra, see

Fig. 14B, and to release the urethra, see Fig. 14A. Figs. 15A and 15B show an embodiment similar to that of Figs. 12A-12C except that the intermediate roller has a changeable diameter to squeeze the urethra, see Fig. 15B, and to release the urethra, see Fig. 15A. Figs. 16A and 16B show an embodiment similar to that of Figs. 10A-10C except that the elements are replaced by two cylindrical rollers positioned on opposite sides of the urethra. Finally, Figs. 17A and 17B show an embodiment substantially similar to that of Figs. 16A and 16B except that the restriction device is turned 90° to form an S-shaped curvature of the urethra.

Fig. 18 shows an example of a hydraulic restriction device 234 for use in accordance with the invention. The restriction device 234 comprises an elongated restriction member 236 having an inflatable cavity 238. A tube 240 connects the cavity 238 to a hydraulic fluid reservoir, not shown. The restriction member 236 may be wrapped around the urethra. Alternatively, two restriction members 236 may be used.

Fig. 19 schematically illustrates how any of the above-described embodiments of the urinary incontinence treatment apparatus of the invention can be implanted in a patient. Thus, an implanted adjustable hydraulic restriction device 234 extends almost completely around the urethra 242 and the urethra ²⁴²~~244~~ to be capable of squeezing the urethra 242 as a single unit. An adjustment device in the form of an inflatable cavity in the restriction device 234 is adapted to adjust the restriction device 234 so that the urine passageway is restricted. An implanted assembly 246 includes a hydraulic fluid reservoir and an operation device (which may include a pump) for distributing hydraulic fluid between the reservoir and the inflatable/contractible cavity of the restriction

device 234 via a fluid conduit 240. A wireless remote control of the apparatus comprises an external signal transmitter 248, which may comprise a hand-held unit, and an implanted signal receiver, which is incorporated in the implanted assembly 246, 5 includes a control unit for controlling the restriction device 234 in response to a control signal from the external transmitter. The signal receiver of the assembly 246 further includes an energizer unit which transforms energy from the control signal transmitted by the external transmitter into 10 electric energy for energy consuming implanted components of the apparatus.

A pressure sensor 250 is implanted for sensing the pressure on the restriction device 234. The control unit of the assembly 246 controls the restriction device 234 to 15 release the urethra 242 in response to the pressure sensor 250 sensing an abnormal high pressure.

There are a number of conceivable alternative embodiments of the invention that give the same result as the above-described embodiments. For example, the microprocessor of the 20 external and implanted, respectively, control units may be replaced by discrete components. The power amplifier of the external control unit may be omitted if the signals generated by the signal generator are strong enough. Therefore, the invention is to be accorded the broadest interpretation of the 25 appended claims to encompass all equivalent structures and assemblies.

CLAIMS

1. A urinary incontinence treatment apparatus, comprising
an adjustable restriction device (2) adapted to engage the
5 urethra or urine bladder of a patient, who suffers from
urinary incontinence, to form a restricted urine passageway in
the urethra or urine bladder, an implantable adjustment device
(5) for adjusting the restriction device (2) to restrict the
urethra or urine bladder to close the urine passageway, or
10 release the urethra or urine bladder to open the urine
passageway, when the restriction device is implanted in the
patient, and an implantable operation device
(6,8;10;12;10,14;76-86) for operating the adjustment device,
characterized in that the operation device comprises a powered
15 operation device.

2. An apparatus according to claim 1, further comprising
a reservoir (4;10;16) implantable in the patient and
containing hydraulic fluid, wherein the operation device
20 (6,8;10;12;10,14;76-86) is adapted to operate the adjustment
device (5) by using the hydraulic fluid of the reservoir.

3. An apparatus according to claim 2, Wherein the
reservoir (4;10;16) contains a predetermined amount of
25 hydraulic fluid.

4. An apparatus according to claim 2, wherein the
adjustment device comprises an expandable cavity (5) in the
restriction device (2), the urine passageway being closed upon
30 expansion of the cavity and open upon contraction of the
cavity, and the hydraulic operation device
(6,8;10;12;10,14;76-86) is adapted to distribute hydraulic

fluid from the reservoir (4;10;16) to expand the cavity, and to distribute hydraulic fluid from the cavity to the reservoir to contract the cavity.

5 5. An apparatus according to claim 4, wherein the reservoir (10) defines a chamber (42;64) for said predetermined amount of fluid and the operation device is adapted to change the size of the chamber.

10 6. An apparatus according to claim 5, wherein the operation device comprises first and second wall portions (48;66) of the reservoir (10) and is adapted to provide relative displacement between the first and second wall portions of the reservoir, in order to change the volume of
15 the chamber (42;64).

 7. An apparatus according to claim 6, wherein the operation device is adapted to provide said relative displacement in response to the pressure in the reservoir.

20

 8. An apparatus according to claim 7, wherein the operation device comprises a pressure controlled hydraulic operation device.

25 9. An apparatus according to claim 8, further comprising an alarm adapted to generate an alarm signal in response to the lapse of a predetermined time period during which the pressure controlling the hydraulic operation device exceeds a predetermined high value.

30

 10. An apparatus according to claim 6, wherein the first and second wall portions of the reservoir (10) are

displaceable relative to each other by magnetic means, hydraulic means, or electric control means, or a combination thereof.

5 11. An apparatus according to claim 6, wherein the operation device is adapted to distribute fluid from the reservoir (10) to the cavity (5) of the restriction device (2) in response to a predetermined first displacement of the first wall portion (48;66) of the reservoir relative to the second wall portion of the reservoir and to distribute fluid from the cavity to the reservoir in response to a predetermined second displacement of the first wall portion relative to the second wall portion.

15 12. An apparatus according to claim 4, wherein the operation device comprises a pump (6,12) adapted to pump fluid between the reservoir (4) and the cavity (5) of the restriction device (2).

20 13. An apparatus according to claim 12, wherein the pump comprises a first activation member for activating the pump to pump fluid from the reservoir (4) to the cavity (5) of the restriction device (2) and a second activation member for activating the pump to pump fluid from the cavity to the reservoir.

 14. An apparatus according to claim 13, wherein the first and second activation members are operable by manual manipulation.

30

 15. An apparatus according to claim 13, wherein at least one of the activation members is adapted to operate when

subjected to a predetermined external pressure.

16. An apparatus according to claim 13, wherein at least one of the first and second activating members are operable by
5 magnetic means, hydraulic means, electric control means or manual manipulation means, or a combination thereof.

17. An apparatus according to any of claims 1-16, wherein the operation device comprises a servo means.

10

18. An apparatus according to any of claims 6, 10 or 12 wherein the operation device comprises a reverse servo.

19. A urinary incontinence treatment apparatus,
15 comprising an adjustable restriction device (2) adapted to engage the urethra or urine bladder of a patient, who suffers from urinary incontinence, to form a restricted urine passageway in the urethra or urine bladder, an implantable adjustment device (5) for adjusting the restriction device (2)
20 to restrict the urethra or urine bladder to close the urine passageway, or release the urethra or urine bladder to open the urine passageway, when the restriction device is implanted in the patient, and an implantable operation device (6,8;10;12;10,14;76-86) for operating the adjustment device,
25 characterised in that the operation device comprises a servo means operatively connected to the adjustment device.

20. An apparatus according to claim 19, wherein the operation device is powered.

30

21. An apparatus according to claim 19, wherein the operation device is manually operated.

22. An apparatus according to claim 19 or 20, wherein the servo means comprises a motor, preferably an electric motor.

5 23. An apparatus according to claim 22, wherein the motor is reversible.

24. An apparatus according to claim 22 or 23, further comprising a gearing connected between the motor and the
10 adjustment device.

25. An apparatus according to any of claims 19-21, further comprising an implantable reservoir (4;10;16) defining a chamber for hydraulic fluid, wherein the operation device is
15 adapted to operate the adjustment device (5) by using the hydraulic fluid of the reservoir.

26. An apparatus according to claim 25, wherein the reservoir (4;10;16) contains a predetermined amount of
20 hydraulic fluid.

27. An apparatus according to any of claims 19-21 or 25-26 wherein the servo means comprises a reverse servo.

25 28. An apparatus according to claims 25 and 27, wherein the the reservoir (204) comprises first and second wall portions and the reverse servo is adapted to provide relative displacement between the first and second wall portions of the reservoir, in order to change the volume of the reservoir.

30

29. An apparatus according to claim 28 and, wherein the reverse servo device is adapted to provide said relative

displacement in response to the pressure in the reservoir.

30. An apparatus according to any of claims 19-29,
wherein the servo means comprises a pressure controlled servo
5 means.

31. An apparatus according to claim 30, further
comprising an alarm adapted to generate an alarm signal in
response to the lapse of a predetermined time period during
10 which the pressure controlling the servo means exceeds a
predetermined high value.

32. An apparatus according to claim 27, wherein the
reverse servo comprises magnetic means, electric means or
15 manual manipulation means or a combination thereof.

33. An apparatus according to claim 28, wherein the
reverse servo comprises hydraulic means (10,14, 76-86).

20 34. An apparatus according to claim 33, wherein the
reverse servo further comprises a servo reservoir defining a
chamber containing servo fluid, and the operation device
comprise first and second wall portions of the servo
reservoir, which are displaceable relative to each other to
25 change the volume of the chamber of the servo reservoir.

35. An apparatus according to claim 34, wherein the first
and second wall portions of the servo reservoir are
displaceable relative to each other by magnetic means,
30 hydraulic means, or electric control means.

36. An apparatus according to claim 33, wherein the

reverse servo comprises a servo reservoir (14) and a fluid supply reservoir (10) connected in a closed system and containing a further predetermined amount of fluid.

5 37. An apparatus according to claim 36, wherein the fluid supply reservoir (10) defines a chamber for the further predetermined amount of fluid and the hydraulic operation device is adapted to change the volume of the chamber and thereby control the amount of fluid in the servo reservoir
10 (14).

38. An apparatus according to claim 37, wherein the fluid supply reservoir (10) comprises first and second wall portions, which are displaceable relative to each other to
15 change the volume of the chamber of the fluid supply reservoir.

39. An apparatus according to claim 38, wherein the fluid supply reservoir (10) increases the amount of fluid in the
20 servo reservoir (14) in response to a predetermined first displacement of the first wall portion of the fluid supply reservoir relative to the second wall portion of the fluid supply reservoir and decreases the amount of fluid in the servo reservoir in response to a predetermined second
25 displacement of the first wall portion of the fluid supply reservoir relative to the second wall portion of the fluid supply reservoir.

40. An apparatus according to any of claims 1 or 19,
30 wherein the adjustment device comprises a hydraulic adjustment device, and further comprising a reservoir implantable in the patient and containing a predetermined amount of hydraulic

fluid, and a conduit providing fluid connection between the reservoir and the hydraulic adjustment device, the operation device being adapted to operate the hydraulic adjustment device by distributing hydraulic fluid through the conduit
5 between the reservoir and the hydraulic adjustment device, the conduit and hydraulic adjustment device being devoid of any non-return valve to permit free flow of hydraulic fluid in both directions in the conduit.

10 41. An apparatus according to claim 40, wherein the reservoir forms a fluid chamber with a variable volume, and the operation device is adapted to distribute fluid from the chamber to the adjustment device by reduction of the volume of the chamber and to withdraw fluid from the adjustment device
15 by expansion of the volume of the chamber.

42. An apparatus according to claim 41, wherein the operation device comprises a motor or a pump.

20 43. An apparatus according to claim 41 or 42, wherein the operation device comprises a movable wall of the reservoir for changing the volume of the chamber.

25 44. An apparatus according to claim 43, wherein the operation device is adapted to change the volume of the chamber by moving the movable wall in response to the pressure in the chamber.

30 45. An apparatus according to claim 5 or 25, further comprising an injection port subcutaneously implantable in the patient and in fluid communication with the chamber.

46. An apparatus according to claim 45, wherein the injection port is integrated in the reservoir.

47. An apparatus according to claim 1 or 19, wherein the
5 restriction device comprises an elongated restriction member
and forming means for forming the restriction member into at
least a substantially closed loop around the urethra or urine
bladder, the loop defining a restriction opening, whereby the
adjustment device is adapted to adjust the restriction member
10 in the loop to change the size of the restriction opening.

48. An apparatus according to claim 47, wherein the
forming means forms the restriction member (2) into a loop
having a predetermined size or a size selected from several
15 predetermined sizes.

49. An apparatus according to claim 47, wherein the
adjustment device is adapted to change the size of the
restriction opening such that the outer circumferential
20 confinement surface of the restriction member is changed.

50. An apparatus according to claim 47, wherein the
adjustment device is adapted to change the size of the
restriction opening such that the outer circumferential
25 confinement surface of the restriction member is unchanged.

51. An apparatus according to claim 47, wherein the
restriction member is non-inflatable, and the adjustment
device is adapted to adjust the restriction member in said
30 loop.

52. An apparatus according to claim 35, wherein the

adjustment device mechanically adjusts the restriction member.

53. An apparatus according to claim 51, wherein the adjustment device hydraulically adjusts the non-inflatable
5 restriction member.

54. An apparatus according to claim 52 or 53, wherein the elongated restriction member (204) is flexible, and the adjustment device (210) is adapted to pull a first portion
10 (204A) of the flexible restriction member from a second portion (204B) of the flexible restriction member opposite the first portion in the loop to squeeze the urethra (206) or urine bladder between two opposite lengths of the elongated flexible restriction member to restrict the passageway, and to
15 release the urethra or urine bladder from the flexible restriction member to enlarge the passageway.

55. An apparatus according to claim 1 or 19, wherein the adjustment device mechanically adjusts the restriction device.
20

56. An apparatus according to any of claims 1 or 19 and 2 or 40 or 55, wherein the restriction device (212) comprises at least two elements (214) to be placed on different sides of the urethra (206) or urine bladder, and the adjustment device
25 is adapted to squeeze the urethra or urine bladder between the elements to restrict the urine passageway in the urethra or urine bladder, and to release the urethra or urine bladder from the elements to enlarge the urine passageway (Figs. 10A, 10B).

30

57. An apparatus according to any of claims 1 or 19, wherein the restriction device (218) comprises at least two

articulated clamping elements (220) to be positioned on opposite or different sides of the urethra (206) or urine bladder, and the adjustment device (222) is adapted to turn the clamping elements toward each other to clamp the urethra or urine bladder between the clamping elements to restrict the urine passageway in the urethra or urine bladder, and to turn the clamping elements away from each other to release the urethra or urine bladder from the elements to enlarge the urine passageway (Fig. 11).

10

58. An apparatus according to any of claims 1 or 19 and 2 or 40 or 55, wherein the restriction device is adapted to bend a portion of the urethra or urine bladder (Figs. 12A-17B).

15

59. An apparatus according to claim 42, wherein the restriction device (224) comprises at least two bending members (226-230) to be positioned on opposite sides of the urethra (206) or urine bladder and to be displaced relative to each other along the urine passageway in the urethra or urine bladder, and the adjustment device (232) is adapted to move the bending members against the urethra or urine bladder to bend the urethra or urine bladder to restrict the urine passageway in the urethra or urine bladder, and to move the bending members away from the urethra or urine bladder to release the urethra or urine bladder from the bending members to enlarge the urine passageway (Figs. 12A-12C).

20

25

60. An apparatus according to claim 43, wherein the bending members comprise rollers.

30

61. An apparatus according to any of claims 1 or 19, wherein the restriction device is adapted to rotate a portion

of the urethra or urine bladder.

62. An apparatus according to any of the preceding claims, further comprising a wireless remote control (44,126,132-144) for non-invasively controlling the hydraulic operation device (6,8;10;12;10,14;76-86).

63. An apparatus according to claim 62, wherein the remote control comprises an external wireless hand-held remote control unit which is manually operable by the patient to control the restriction device to squeeze or release the urethra or urine bladder.

64. An apparatus according to claim 62, wherein the remote control (44,126,132-144) comprises an external signal transmitter (132,136), receiver or transceiver and a signal receiver (134,138), transmitter or transceiver implantable in the patient.

65. An apparatus according to claim 64, wherein the signal receiver (134,138) and/or transmitter comprises a control unit (138) adapted to control the operation device (6,8;10;12;10,14;76-86) in response to a control signal received from the signal transmitter (132, 136).

66. An apparatus according to claim 65, further comprising an implantable energizer unit (136) for providing energy to energy consuming implantable components of the apparatus.

67. An apparatus according to claim 1 or 19 or 66, wherein the operation device comprises a motor (44) for

operating the adjustment device.

68. An apparatus according to claims 66 and 67, wherein the control unit (138) is adapted to power the motor (44) with energy provided by the energizer unit (136) in response to a control signal received from the signal transmitter (132,136).

69. An apparatus according to claim 62, wherein the remote control (44,126,132-144) comprises wireless energy transfer means for transferring energy from outside the patient's body to energy consuming implantable components of the apparatus.

70. An apparatus according to claim 66 and 69, wherein the energy transfer means comprises an implantable energizer unit (126), which is adapted to transform energy from the control signal, as it is transmitted to the signal receiver (134,138), into electric energy.

71. An apparatus according to claim 69, wherein the operation device (6;8;10;12;10,14;76-86) comprises a motor (44), and the wireless energy transfer means is adapted to directly power the motor with transferred energy.

72. An apparatus according to claim 70 or 71, wherein the energy transferred by the wireless energy transfer means comprises a signal.

73. An apparatus according to claim 72, wherein the signal comprises a wave signal.

74. An apparatus according to claim 70 or 71, wherein the

energy transferred by the wireless energy transfer means comprises an electric field or a magnetic field or a combination thereof.

5 75. An apparatus according to claim 72, wherein the signal is analog or digital or a combination thereof.

 76. An apparatus according to claim 64 or 65, wherein the signal transmitter (132,136) and signal receiver (134,138) are adapted to transmit and receive an analog or digital signal or a combination thereof.

 77. An apparatus according to claim 75 or 76, wherein the signal comprises analog or digital pulses.

15 78. An apparatus according to any of claims 75-77, wherein the analog or digital signal comprises a magnetic field or an electric field or a combination thereof.

20 79. An apparatus according to claim 64 or 65, wherein the signal transmitter (132,136) and signal receiver (134,138) are adapted to transmit and receive a wave signal.

 80. An apparatus according to claim 72 or 79, wherein the wave signal comprises an electromagnetic wave signal, a sound wave signal or a carrier wave signal for a remote control signal or a combination thereof.

 81. An apparatus according to claim 80, wherein the carrier signal is frequency, amplitude or frequency and amplitude modulated.

82. An apparatus according to claim 72 or 75 wherein the energy transfer means transfers the energy from the signal into a direct, pulsating direct or alternating current or a combination thereof.

5

83. An apparatus according to claim 62, wherein the remote control (44,126,132-144) is capable of obtaining information related to important parameters of the apparatus from inside the patient's body and of commanding the adjustment device (5) to adjust the restriction device (2) in response to obtained information.

10

84. An apparatus according to claim 62, wherein the remote control is capable of obtaining information related to the urine passageway in the urethra or urine bladder and of commanding the adjustment device to adjust the restriction device in response to obtained information.

15

85. An apparatus according to claim 1 or 19 or 40 or 2 or 55, further comprising an implantable source of energy for powering the operation device and/or for energizing other energy consuming components of the apparatus, wherein the energy from the source of energy is releasable from outside the patient's body.

20

25

86. An apparatus according to claim 1 or 19 or 40 or 2 or 55, further comprising an energy transmission device for wireless transmission of energy.

30

87. An apparatus according to claim 85 and 86, wherein the energy transmission device transmits energy of a first form, and further comprising an energy transforming device

implantable in the patient for transforming the energy of the first form into energy of a second form, to be supplied to the source of energy and/or other implantable energy consuming parts of the apparatus.

5

88. An apparatus according to claim 87, wherein the energy of the second form is different than the energy of the first form.

10

89. An apparatus according to claim 87, wherein the energy transmission device functions different from the energy transforming device.

90. An apparatus according to claim 86, further comprising an implantable motor or pump for operating the adjustment device, wherein the energy transmission device is adapted to transmit wireless energy in the form of an magnetic field or electromagnetic waves or field for direct power of the motor or pump, as the wireless energy is being transmitted.

15
20

91. An apparatus according to claim 65 and 86, wherein the energy transmission device transmits energy by at least one signal separate from the control signal.

25

92. An apparatus according to claim 87, further comprising an implantable stabiliser for stabilising the energy of the first or second form.

30

93. An apparatus according to claim 92, wherein the energy of the second form comprises electric current and the stabiliser comprises at least one capacitor.

94. An apparatus according to any of claims 85,87-89,
wherein the source of energy comprises a battery, accumulator,
5 capacitor or a combination thereof.

95. An apparatus according to claim 1 or 19 or 40 or 2 or
55, further comprising a control device adapted to produce
wireless energy for directly powering the operation device
10 and/or for energizing other energy consuming components of the
apparatus.

96. An apparatus according to claim 1 or 19 or 40 or 2 or
55, further comprising an implantable energy transforming
15 device for transforming wireless energy directly or indirectly
into energy different than the wireless energy for operation
of the restriction device.

97. An apparatus according to claim 95 or 96, wherein
20 the wireless energy comprises a wave signal including a sound
wave signal, an ultrasound wave signal, an electromagnetic
wave signal, an infrared light signal, a visible light signal,
an ultra violet light signal, a laser light signal, a micro
wave signal, a radio wave signal, an x-ray radiation signal or
25 a gamma radiation signal.

98. An apparatus according to claim 1 or 19 or 95,
further comprising an energy transfer means (22,326,332-344)
for wireless transfer of energy from outside the patient's
30 body to the operation device or adjustment device and/or other
energy consuming implantable components of the apparatus.

99. An apparatus apparatus according to claim 95, wherein the control device is adapted to produce wireless energy in the form of a train of energy pulses.

5 100. An apparatus according to claim 69 or 98, wherein the energy transfer means is adapted to intermittently transfer the energy in the form of a train of energy pulses for direct use in connection with the energising of the energy consuming components of the apparatus.

10

101. An apparatus according to claim 95 and 87 wherein the control device is adapted to control the energy transforming device to produce the energy of the second form in a train of energy pulses for direct use in connection with
15 the operation of the adjustment device.

102. An apparatus according to claim 100 or 101, wherein the energy transfer device is adapted to transfer electric energy, and further comprising an implantable capacitor for
20 producing the train of energy pulses.

103. An apparatus according to claim 102 or 93,94, wherein the capacitor has a capacity less than 0,1 μ F.

25 104. An apparatus according to claim 98, further comprising an implantable motor (22) or pump for operating the adjustment device (12;52;66;90,92;104;110), wherein the energy transfer means is adapted to directly power the motor or pump with transferred energy.

30

105. An apparatus according to claim 90 or 104, wherein the pump is not a plunger type of pump.

106. An apparatus according to claim 1 or 19 or 40 or 2
or 55, wherein the adjustment device is adapted to adjust the
restriction device in a non-manual, non-thermal or non-
5 magnetic manner.

107. An apparatus according to any of claims 63-106,
further comprising a wireless remote control (44,126,132-144)
for non-invasively controlling the operation device
10 (6,8;10;12;10,14;76-86).

108. An apparatus according to any one of the preceding
claims, wherein the operation device is electrically powered.

15 109. An apparatus according to claim 1 or 19 or 90,
wherein the operation device is unpowerable by static
permanent magnetic energy.

110. An apparatus according to claim 1 or 19 or 40 or 2
20 or 55, wherein the operation device is adapted to non-
invasively operate the adjustment device.

111. An apparatus according to claim 1 or 19 or 40 or 2
or 55, wherein the adjustment device is operable to adjust the
25 restriction device to steplessly change the restriction of the
urine passageway.

112. An apparatus according to claim 1 or 19 or 40 or 2,
wherein the operation device comprises a hydraulic operation
30 device which uses hydraulic fluid, the viscosity of which
changes when the hydraulic fluid is exposed to energy
different than thermal energy.

113. An apparatus according to claim 108, wherein the viscosity of the hydraulic fluid changes when the fluid is exposed to electric energy.

5

114. An apparatus according to claim 1 or 19, further comprising an adjustment device for adjusting the restriction device to change the restriction of the urine passageway, wherein the adjustment device is adapted to mechanically
10 adjust the restriction device, or adapted to hydraulically adjust the restriction device by using hydraulic means which is devoid of hydraulic fluid of the kind having a viscosity that substantially increases when exposed to heat or a magnetic field.

15

115. An apparatus according to claim 1 or 19, further comprising a control device for controlling the restriction device.

20

116. An apparatus according to claim 115, wherein the control device comprises an internal control unit implantable in the patient for controlling the restriction device.

25

117. An apparatus according to claim 116, wherein the internal control unit is programmable.

118. An apparatus according to claim 117, wherein the control device comprises an external control unit outside the patient's body, the implantable internal control unit being
30 programmable by the external control unit.

119. An apparatus according to claim 115, wherein the

control device comprises an external control unit outside the patient's body for wirelessly controlling the restriction device.

5 120. An apparatus according to claim 119, wherein the external control unit is programmable.

121. An apparatus according to any one of the preceding claims, further comprising at least one implantable sensor for
10 sensing at least one physical parameter of the patient.

122. An apparatus according to claim 121, wherein the sensor is adapted to directly or indirectly sense as the physical parameter the horizontal position of the patient.
15

123. An apparatus according to claim 121, wherein the sensor comprises a pressure sensor for directly or indirectly sensing as the physical parameter the pressure against the restriction device or part of the human body.
20

124. An apparatus according to claim 123, wherein the restriction device is adapted to enlarge the urine passageway in the urethra or urine bladder in response to the pressure sensor sensing a predetermined pressure.
25

125. An apparatus according to any one of claims 121-124, further comprising a control device for controlling the restriction device in response to signals from the sensor.

30 126. An apparatus according to claim 125, wherein the control device comprises an internal control unit implantable in the patient and directly controlling the restriction device

in response to signals from the sensor.

127. An apparatus according to claim 126, wherein the control device comprises an external control unit outside the patient's body for controlling the restriction device in response to signals from the sensor.

128. An apparatus according to claim 126, wherein the control device comprises an external control unit outside the patient's body for manually controlling the restriction device in response to information from the sensor.

129. An apparatus according to claim 115, further comprising an implantable source of energy, wherein the control device is operable from outside the patient's body for controlling the source of energy to release energy for use in connection with the operation of the prosthesis, when the prosthesis is implanted.

130. An apparatus according to claim 129, wherein the source of energy is intended to be external to the patient's body, and the control device is adapted to control the external source of energy to release wireless energy for use in connection with the operation of the prosthesis.

131. An apparatus according to claim 129, wherein the control device controls the source of energy to release magnetic energy, non-magnetic energy, electromagnetic energy, non-electromagnetic energy, kinetic energy, non-kinetic energy, sonic energy, non-sonic energy, thermal energy or non-thermal energy.

132. An apparatus according to claim 1 or 19 or 40 or 2
or 55, wherein the operation device is powered by magnetic
energy, non-magnetic energy, electromagnetic energy, non-
electromagnetic energy, kinetic energy, non-kinetic energy,
5 sonic energy, non-sonic energy, thermal energy or non-thermal
energy.

133. An apparatus according to claim 129, wherein the
control device controls the source of energy to release energy
10 for a determined time period.

134. An apparatus according to claim 129 or 129 and 99,
wherein the control device controls the source of energy to
release energy in a determined number of energy pulses .
15

135. An apparatus according to claim 129, wherein the
control device is adapted to control the source of energy to
release energy in a non-invasive manner.

20 136. An apparatus according to claim 1 or 19 or 40 or 2
or 55, further comprising implantable electrical components
including at least one voltage level guard.

137. An apparatus according to claim 1 or 19 or 40 or 2
25 or 55, further comprising implantable electrical components
including a single voltage level guard.

138. An apparatus according to claim 136 or 137, wherein
the electrical components are devoid of any current detector
30 and/or charge level detector.

139. An apparatus according to any of claims 85, 102, 87,

93 or 94 and 136-138, further comprising an implantable capacitor or accumulator, wherein the charge or discharge of the capacitor or accumulator is controlled by use of the voltage level guard.

5

140. An apparatus according to claim 65, 70 or 91, wherein the control signal comprises a wave signal including a sound wave signal, an ultrasound wave signal, an electromagnetic wave signal, an infrared light signal, a
10 visible light signal, an ultra violet light signal, a laser light signal, a micro wave signal, a radio wave signal, an x-ray radiation signal or a gamma radiation signal.

141. An apparatus according to any of the preceding
15 claims, further comprising a switch implantable in the patient for directly or indirectly switching the operation of the restriction device.

142. An apparatus according to claim 141 and 86, further
20 comprising a source of energy implantable in the patient for supplying energy for the operation of the restriction device, wherein the switch is operated by the energy supplied by the energy transmission device to switch from an off mode, in which the source of energy is not in use, to an on mode, in
25 which the source of energy supplies energy for the operation of the restriction device.

143. An apparatus according to claim 141 and 86, further comprising a source of energy implantable in the patient for
30 supplying energy for the operation of the restriction device, and a remote control for controlling the supply of energy of the implantable source of energy, wherein the switch is

operated by the energy supplied by the energy transmission device to switch from an off mode, in which the remote control is prevented from controlling the source of energy and the source of energy is not in use, to a standby mode, in which
5 the remote control is permitted to control the source of energy to supply energy for the operation of the restriction device.

144. An apparatus according to claim 141 and 87, further
10 comprising a source of energy implantable in the patient for supplying energy for the operation of the restriction device, wherein the switch is operated by the energy supplied by the energy transforming device to switch from an off mode, in which the source of energy is not in use, to an on mode, in
15 which the source of energy supplies energy for the operation of the restriction device.

145. An apparatus according to claim 141 and 87, further comprising a source of energy implantable in the patient for
20 supplying energy for the operation of the restriction device, and a remote control for controlling the supply of energy of the implantable source of energy, wherein the switch is operated by the energy supplied by the energy transforming device to switch from an off mode, in which the remote control
25 is prevented from controlling the source of energy and the source of energy is not in use, to a standby mode, in which the remote control is permitted to control the source of energy to supply energy for the operation of the restriction device.

30

146. An apparatus according to claim 1 or 19 or 40 or 2 or 55, wherein the prosthesis is operable to perform a

reversible function.

147. An apparatus according to claim 67 or 146, further comprising a reversing device implantable in the patient for
5 reversing the function performed by the prosthesis.

148. An apparatus according to claim 147, wherein the control device controls the reversing device to reverse the function performed by the prosthesis.
10

149. An apparatus according to claim 147, wherein the reversing device comprises hydraulic means including a valve for shifting the flow direction of a flowing fluid in the hydraulic means.
15

150. An apparatus according to claim 147, wherein the reversing device comprises a mechanical reversing device.

151. An apparatus according to claim 147, wherein the
20 reversing device comprises a switch.

152. An apparatus according to claim 151, wherein the switch of the reversing device is operable by the released energy.
25

153. An apparatus according to claim 152, wherein the control device controls the operation of the switch of the reversing device by shifting polarity of the released energy supplied to the switch.
30

154. An apparatus according to claim 147, wherein the operation device comprises a motor, and the reversing device

reverses the motor.

155. An apparatus according to any of the preceding claims, wherein the restriction device is embedded in a soft
5 or gel-like material.

156. An apparatus according to claim 155, wherein the restriction device is embedded in a silicone material having hardness less than 20 Shore.

10

157. An apparatus according to claim 87, wherein the energy transforming means or device is designed to be implanted subcutaneously or in the abdomen, thorax or cephalic region of the patient.

15

158. An apparatus according to any of the preceding claims, wherein the adjustment device is adapted to adjust the restriction device such that the restriction device provides a predetermined contraction of the faecal passageway that is
20 satisfactory for the patient.

159. An apparatus according to claim 1 or 19, wherein the adjustment device is adapted to adjust the restriction device in a non-flux magnetic, non-thermal or non-viscosity changing
25 manner.

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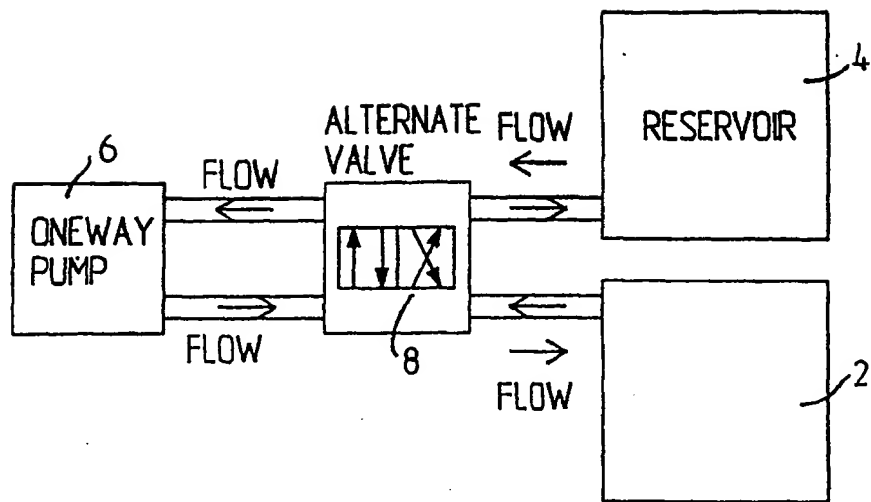


FIG.1A

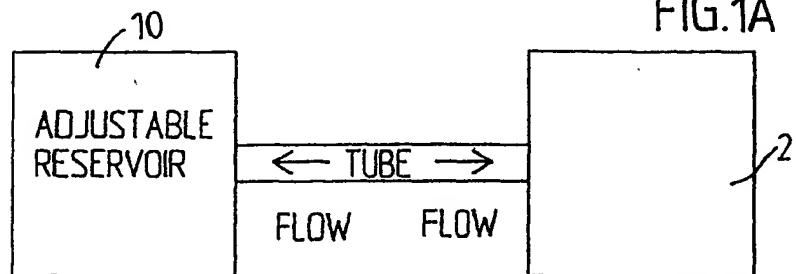


FIG.1B

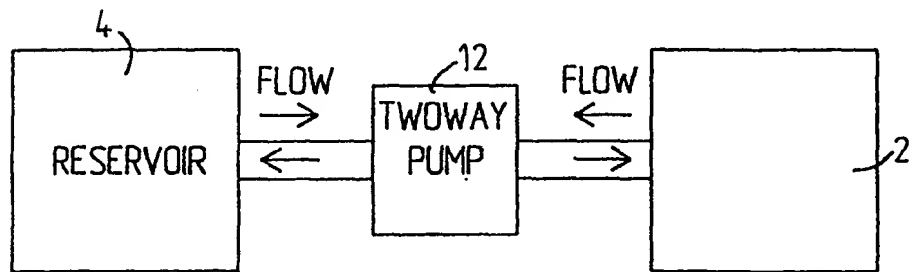


FIG.1C

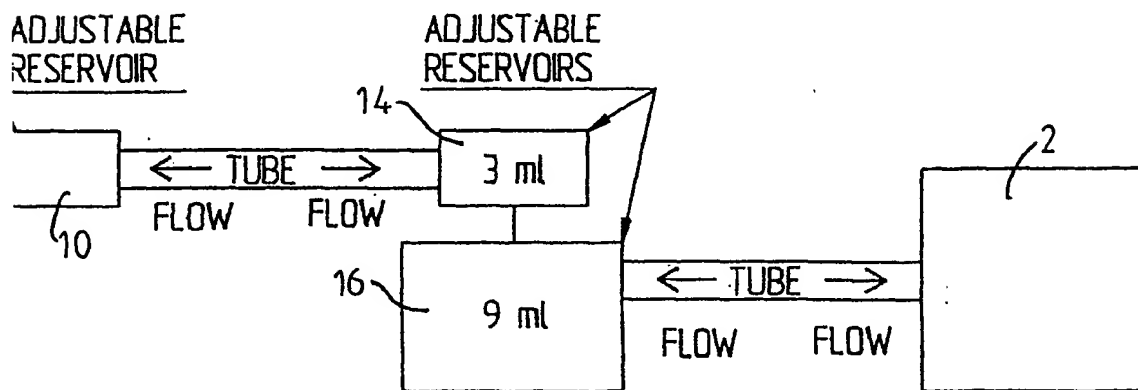
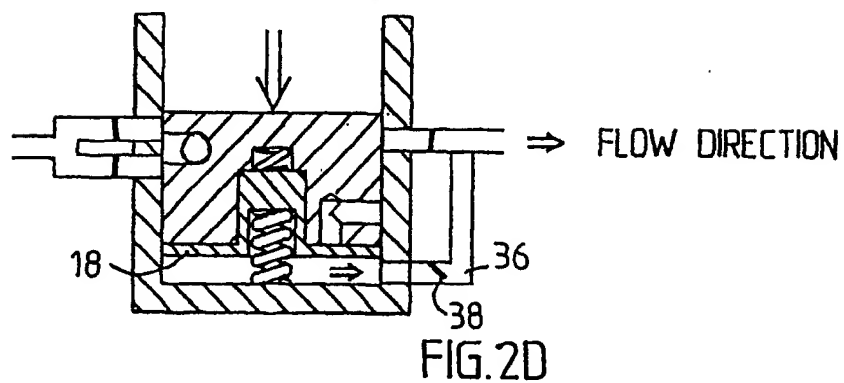
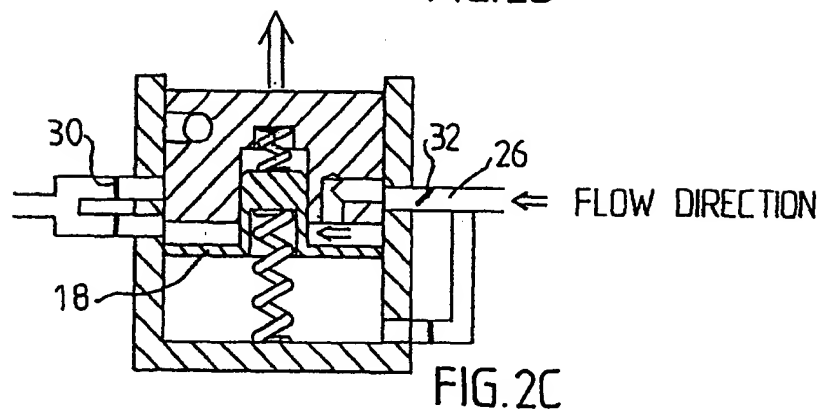
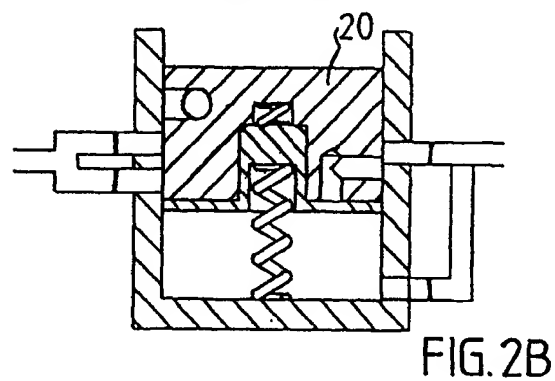
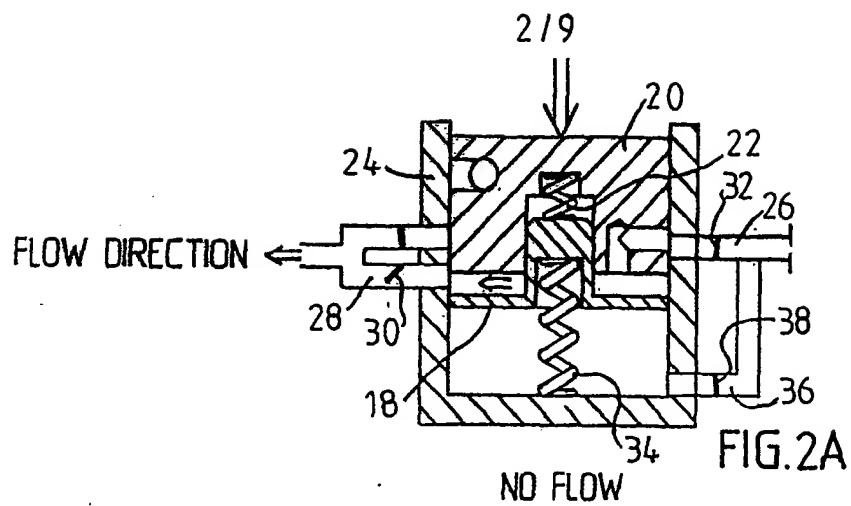
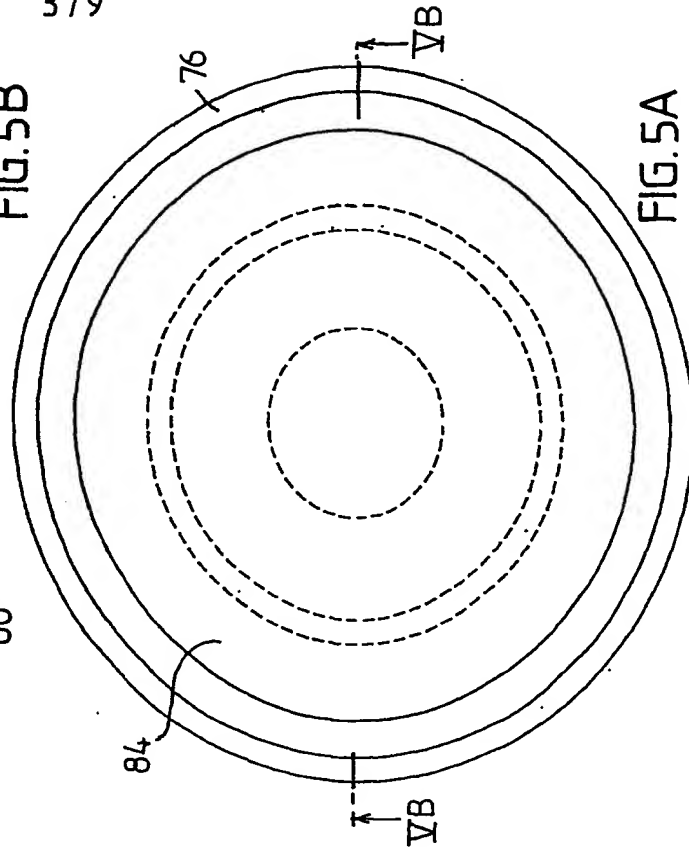
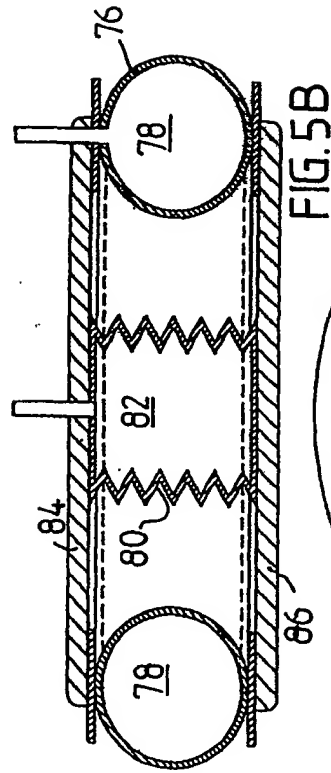
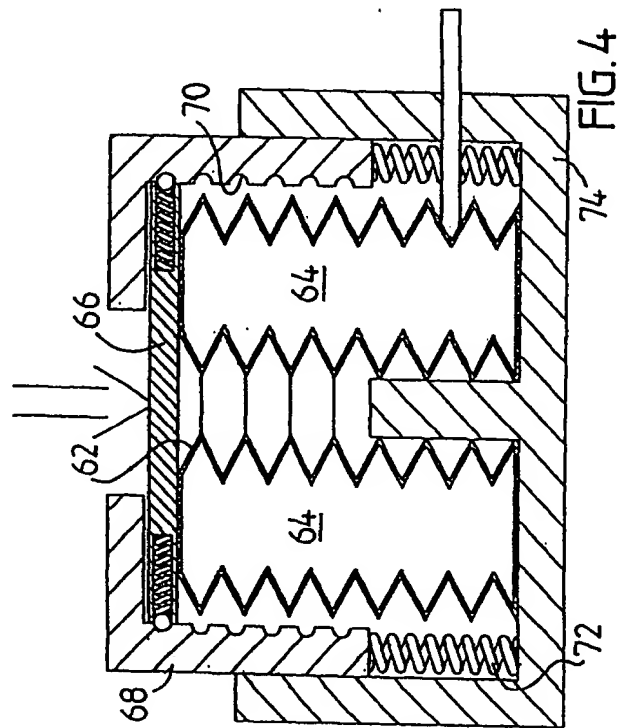
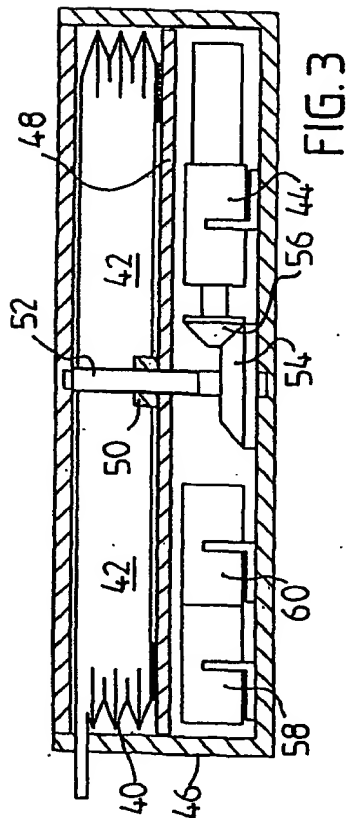
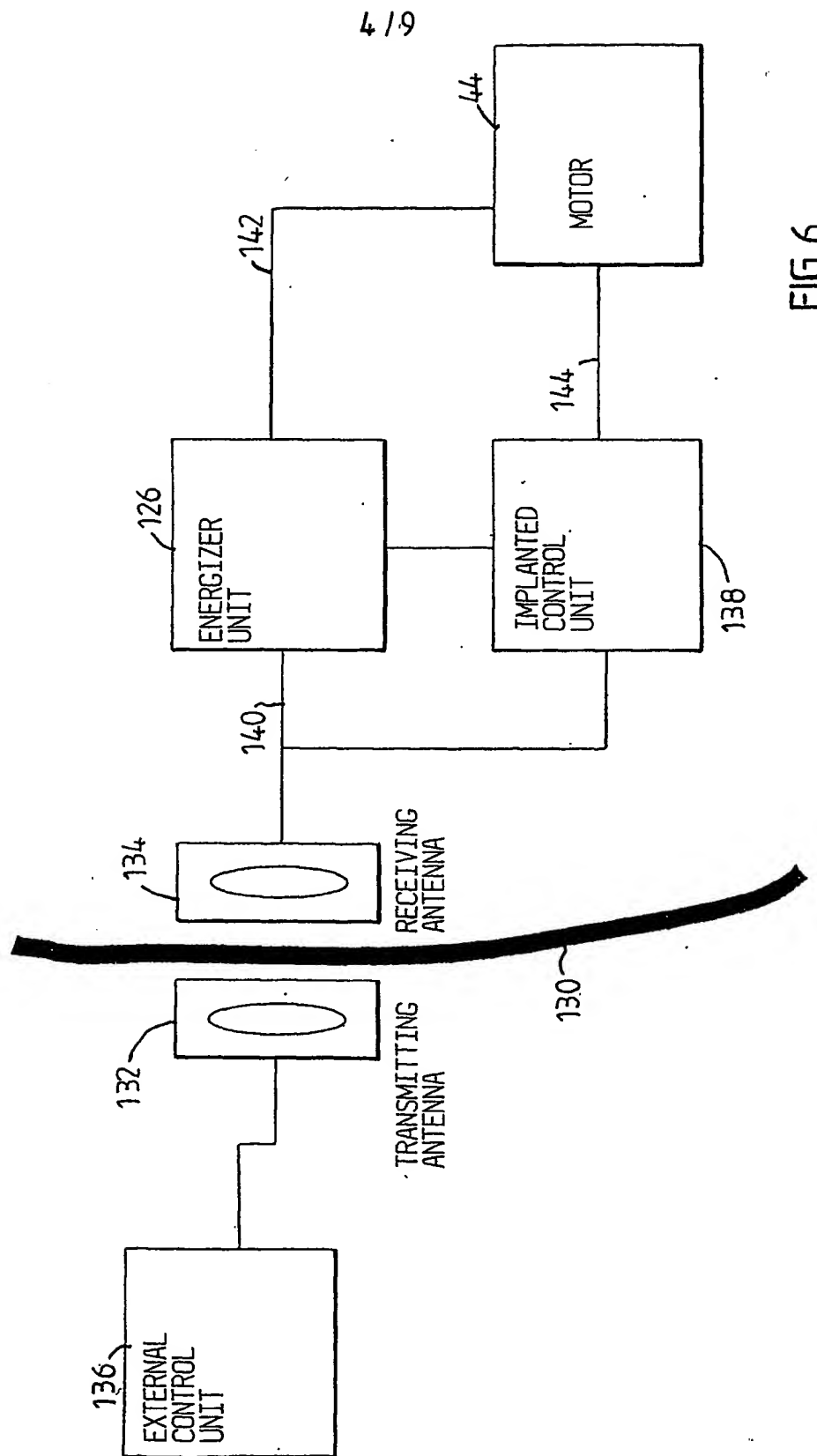


FIG.1D



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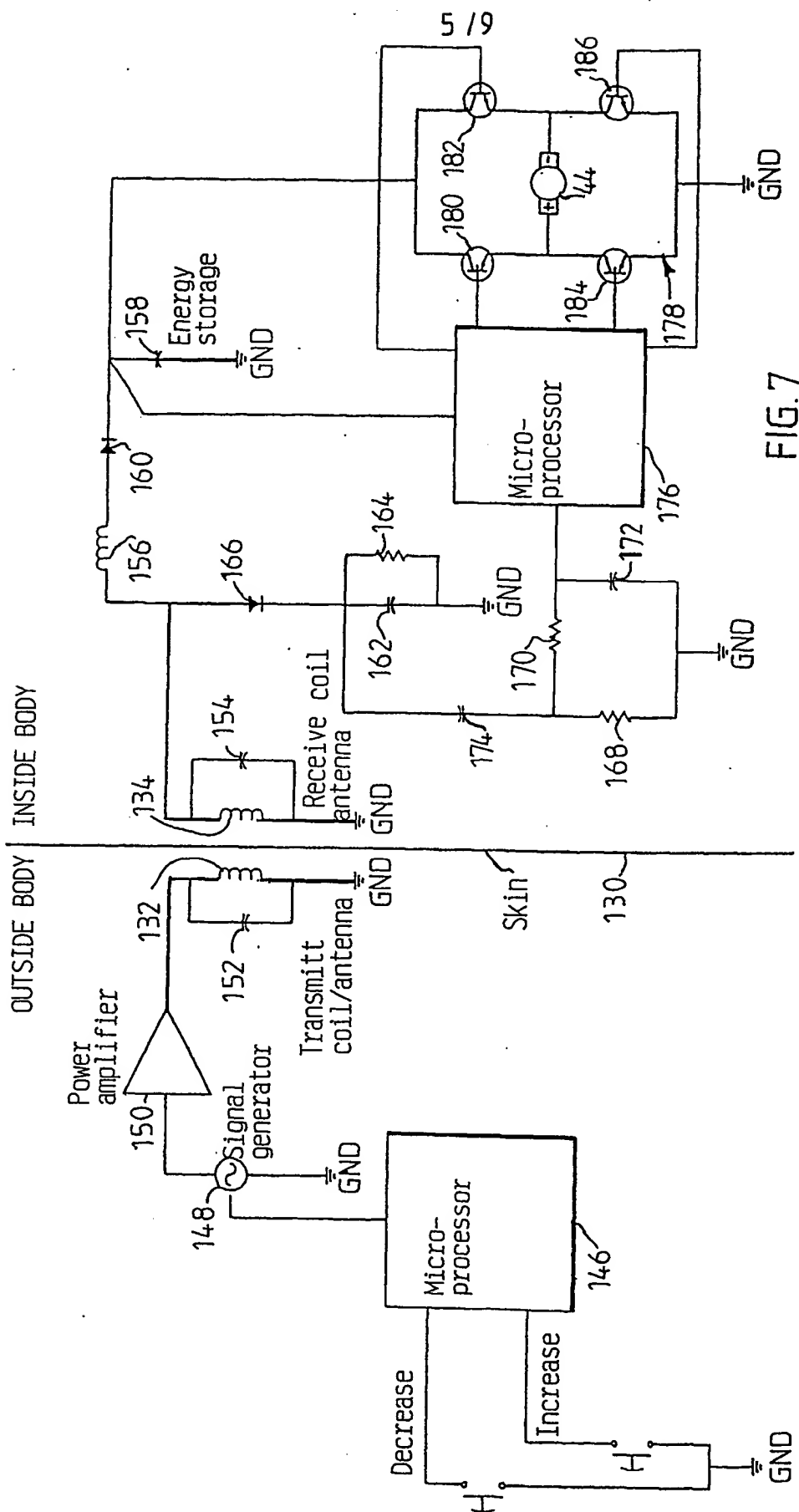


FIG. 7

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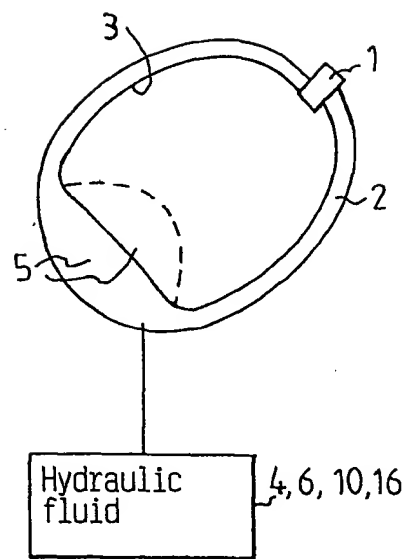


FIG. 8

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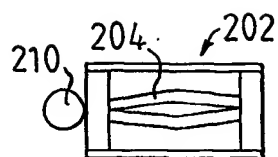


FIG. 9A

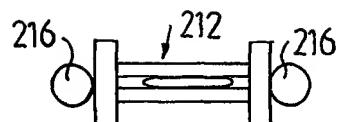


FIG. 10A

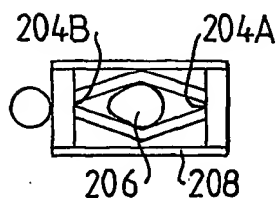


FIG. 9B

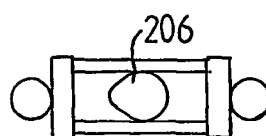


FIG. 10B

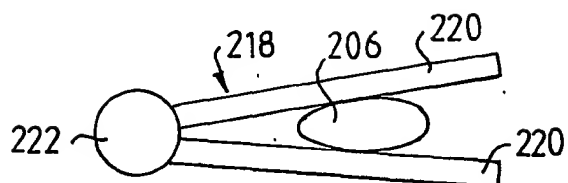


FIG. 11

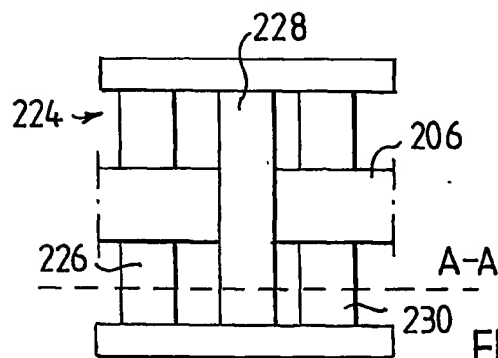


FIG. 12A

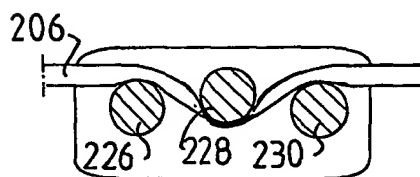


FIG. 12B

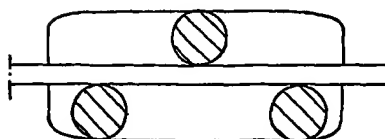


FIG. 12C

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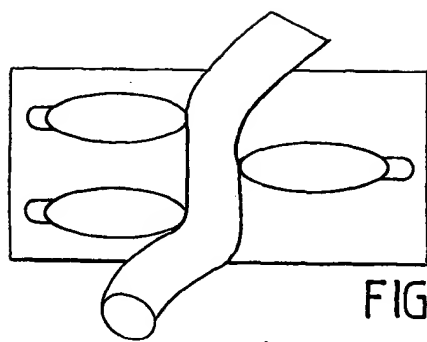


FIG. 13A

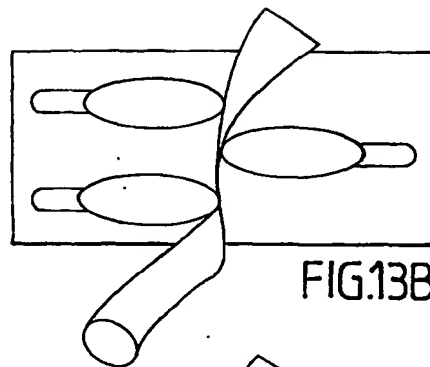


FIG. 13B

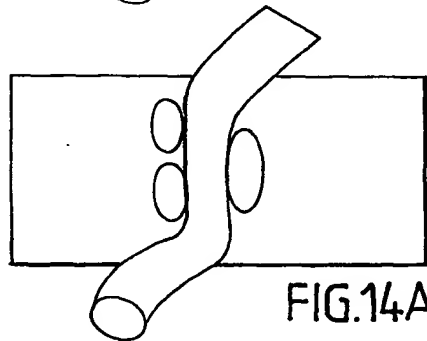


FIG. 14A

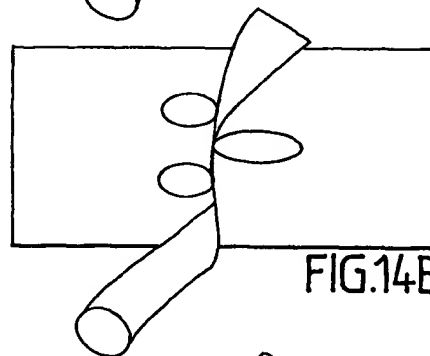


FIG. 14B

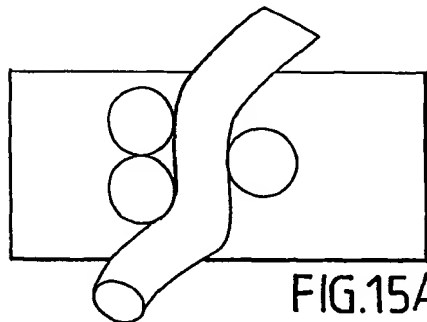


FIG. 15A

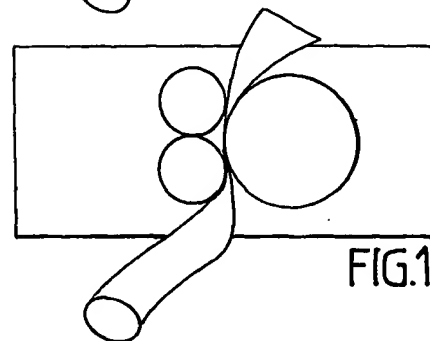


FIG. 15B

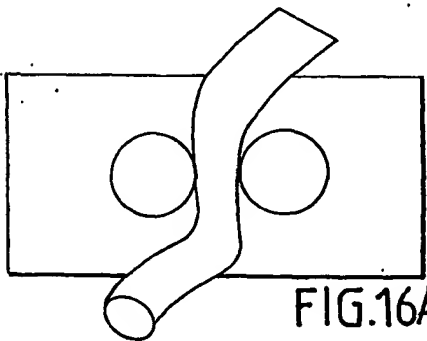


FIG. 16A

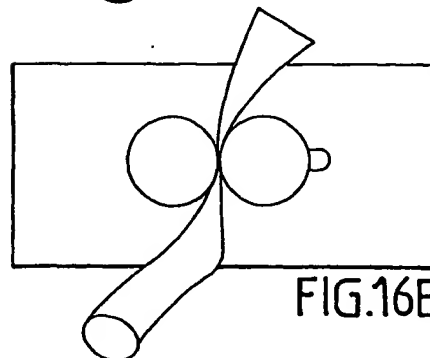


FIG. 16B

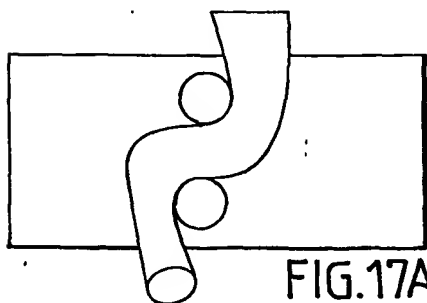


FIG. 17A

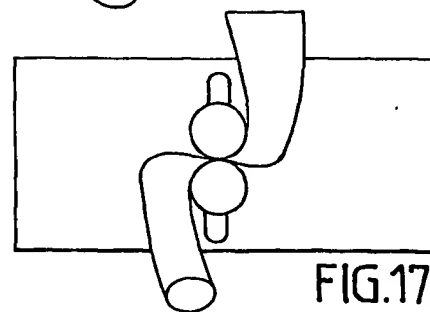


FIG. 17B

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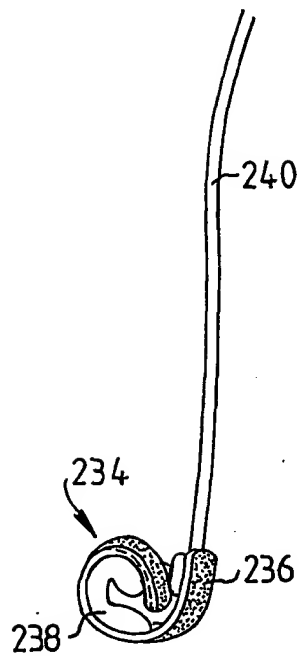


FIG. 18

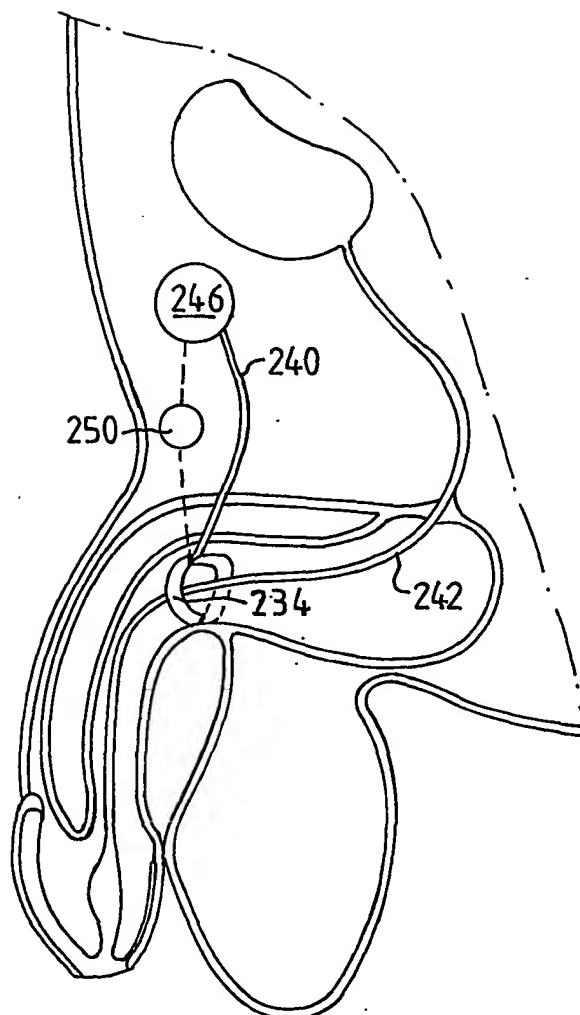
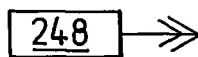


FIG.19